Joint moment loading interplay between the shoulders and the low back during patient handling in nurses

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Abstract.

BACKGROUND: Manual patient handling completed by nurses can include unexpected or strenuous exertions, potentially leading to injury. Lifting guidelines focus on mitigating primarily limiting low back exposures, and the influence of these techniques on the shoulder is unknown.

OBJECTIVE: To quantify shoulder loading during manual patient handling tasks and determine whether approaches intended to limit low back exposures negatively affect shoulder demands.

METHODS: Twenty novice university-aged females completed five manual patient handling tasks before and after a training session. Participants simulated handling a partial weight bearing patient, and joint load magnitudes were calculated. Strength demands were interpreted in the context of available population capability ranges.

RESULTS: Using recommended techniques decreased peak low back loading in most scenarios ($p = 0.01–0.02$), but had variable effects on shoulder loading. Peak loading in the shoulders increased by 97–107% in the Sit-to-Chair task following training. Using recommended techniques for Turn Toward decreased mean population strength requirements at the back to 35% of capability while increasing shoulder requirements to 100% capability.

CONCLUSIONS: Recommended manual patient handling techniques mitigate low back exposures but likely transfer demands to other body regions, specifically the shoulder.

Keywords: Nursing, manual patient handling, upper extremity, joint loading

1. Introduction

Manual materials handling is often associated with manufacturing and warehousing, but non-traditional load handling scenarios exist in other workplaces, and are accompanied by the same musculoskeletal overexertion potential. Indeed, the manual patient handling completed by nurses requires transferring or repositioning substantially more complicated, unmodifiable, and often heavier objects.

Differences in anthropometrics, ability to assist, or combative and uncooperative patients can result in unexpected or strenuous exertions, leading to injury risk [1–3]. Health care and social services are second only to manufacturing sectors in Ontario for lost time injury claims [4], and musculoskeletal disorders are the cause for $\sim 50\%$ of injuries in this group, nine times the US national rate [5].
Injury rates led to extensive research and creation of standardized lifting practices, but adoption of these practices can be slow, and practices focus almost exclusively on the low back. Specific tasks, including turning, repositioning or transferring a patient are recognized as high-demand activities, producing greater than recommended spinal compression forces [6–9]. The dangers associated with manual patient handling have led many health units to adopt safe lifting policies, and in some cases banning certain patient handling tasks [3]. Mechanical lifting devices and lifting techniques have effectively reduced low back injuries and lost days from work [2,9,10]. Despite these advances, manual patient handling continues to be completed by nurses who cite a lack of time, unfamiliarity with the manual devices and a lack of available equipment as reasons for favouring manual transfers [11–13]. Widespread adoption of these techniques can be slow; previous research has indicated that up to 46% of registered nurses either were not informed or aware of national safe patient handling and mobility standards [14]. While nurses receive training throughout their undergraduate careers as well as on the job training, they often mimic the lifting techniques performed by more experienced persons [15,16]; which may result from the new nurse wanting to assimilate and avoid confrontation. Thus, new nurses may continue to use suboptimal techniques and promote these strategies amongst subsequent nursing generations [17,18].

While developed strategies have reduced low back injury in nurses, the influence of these techniques on the shoulder is unknown. As these ergonomic interventions have focused chiefly on the low back, concerns exist regarding potential physical demand transfers between joint in manual patient handling [19–21]. Some tasks, such as shifting the patient up or down the bed or turning the patient to one side, are highly demanding of the shoulder [20]. Other intended ergonomics interventions reduced perceived exertion at the low back while increasing it at the shoulder [2,10]. Shoulder injuries in manual patient handling remain common among nurses. The focus of this work is to quantify shoulder loading during manual patient handling tasks and determine whether approaches intended to reduce low back exposures concomitantly increase shoulder demands. We hypothesized that trained manual patient handling techniques would decrease low back loading, but would increase peak joint moments observed at the shoulders.

2. Methods

2.1. Participants

Twenty healthy university-aged females (21.6 ± 1.3 years; 1.66 ± 0.07 m tall; 62.5 ± 9.4 kg body weight) participated. Exclusion criteria were injury or pain in the past year to the upper extremity or back and previous experience or training in manual patient handling. Participants provided informed consent prior to collection, and the institutional Office of Research Ethics approved the study.

2.2. Instrumentation

Motion capture data was collected for all experimental trials. Three-dimensional motion was tracked using an 8-camera Vicon MX20 system (VICON, Oxford, UK). Individual markers were placed over anatomical landmarks: bilaterally over the 2nd and 5th metacarpals, radial and ulnar styloidis, medial and lateral epicondyles, acromii, and posterior superior iliac spine, as well as on the suprasternal notch, xiphoid process, and 5th lumbar spinous process. A static calibration frame established relationships between clusters and anatomical landmark markers, allowing subsequent construction of segment coordinate systems and joint centers [22]. Kinematics were sampled at 50 Hz using VICON Nexus 1.2.1 software (Oxford, UK).
To quantify resultant joint moments at the shoulders and low back, forces generated at the hand were estimated following each set of manual patient handling trials. Two ErgoFet 300\textsuperscript{TM} uniaxial hand dynamometers (Hogan Health Industries, Utah, USA) were used to record hand force estimates for each task. Before collection, participants were calibrated with the dynamometers to determine left and right hand maximum pushes and pulls in similar postures as they assumed in experimental trials to improve accuracy [23]. This calibration involved familiarization of the exertion levels required to attain 25\%, 50\% and 75\% of their maximal force outputs.

2.3. Experimental design

Participants performed defined manual patient handling tasks in two sessions on the same day, before and after a training session. The training session included a self-paced computer presentation of recommended techniques (described graphically and verbally) and videos of recommended lifting strategies for each task. Each video included a practicing nurse with 15 years of experience demonstrating the recommended techniques. The training session finished with physical familiarization and practice with the techniques, including manipulating the patient and feedback from the instructor. Task-specific recommended techniques were extracted from the literature [9,24] (Fig. 1).

2.4. Protocol

The protocol involved application of reflective markers and hand force calibration, a pre-training session, training of recommended techniques, then a post-training session. Within each session, five tasks
were block-randomized and performed three times each for a total of 30 trials (15 pre- and post-training), with rest breaks of up to 5 minutes between tasks. The five tasks analysed were: turning the patient toward and away from the nurse (Turn Toward and Turn Away, respectively), moving the patient upward on the bed (Reposition), moving the patient from supine to sitting on the edge of the bed (Lie-to-Sit), and transferring the patient from sitting on the bed to sitting on an adjacent chair (Sit-to-Chair).

Task conditions were consistent across participants. Each trial was completed on an electrically adjustable cushioned table (56–88 cm above the floor) covered in a slider sheet similar to those found in hospitals. Table height was placed at any height the participant chose during untrained trials, while participants used their waist height in post-training trials, except for the Sit-to-Chair task when the height of the table was moved to match the height of the seat pan of the chair. A 92-kg male was used as the “patient” throughout data collection, and was 87th percentile based on anthropometry tables for weight, and 72nd percentile for stature [25]. The patient simulated a partial weight bearing patient, and only supported himself when in a seated or standing position. The participant always approached the bed on the left, with the head of the patient to the left and feet to the right. Before the pre-training session, the participant was given time to decide on their self-selected technique for moving the patient, along with instruction on the starting and ending patient positions for each task and the opportunity to attempt a few transfers. Specific instructions following training were emphasized during the post-training trials, including guidance to stay as close to the bed as possible in an effort to minimize external load moment arms at the shoulder and back, to count to three in preparation for each trial, and to shift their body weight between their feet on each count.

Each trial commenced when the participant moved toward the patient after a starting signal. Participants had 15 seconds to complete the Turn Away, Turn Toward, and Reposition tasks and 25 seconds for the Lie-to-Sit and Sit-to-Chair trials. Trials lengths were established through pilot testing to provide sufficient time to perform each transfer at a typical self-selected pace. Once three repetitions of each task were completed, hand force estimations immediately followed. Participants verbally reported how hard they were working as a percentage of their maximum, in addition to verbally reporting how their exertion was distributed between their hands (e.g. 70% left vs 30% right). They then used the hand force dynamometers against a secured bar to replicate estimated hand forces, with hand force direction relative to the hand, task performance height and orientation relative to the participant taken into consideration.

2.5. Data analysis

Kinetic analysis consisted of data filtering, marker reconstruction, local joint coordinate system construction, and external joint moment calculations. Static calibration trials were completed prior to experimental trials, allowing reconstruction in subsequent frames. All raw kinematic data were low-pass filtered with a frequency of 6 Hz [26], and segment lengths and orthogonal coordinate systems were completed using ISB standards [27]. Locations of joint centres, along with participant weight, stature and estimated hand forces were used as inputs in a top-down inverse quasi-static model (similar to that of Dickerson et al. [28]) to determine time series moment data of the left and right shoulder as well as the low back. The recorded force from the hand force estimations was used throughout the trials. In order to prevent non-task movements from being considered, each trial was visually examined, and analysis was only completed on relevant frames. Peak resultant (vector norm) moments from each shoulder and the low back were then extracted for analysis.

Michigan’s 3D static strength prediction program (3DSSPP, University of Michigan, Ann Arbor, MI, USA) was used to compare median (50th percentile) population strength requirements to the untrained
and trained condition demands. Video analysis of the self-selected techniques revealed that many participants selected similar styles for each task. Two styles were chosen for self-selected Lie-to-Sit, Sit-to-Chair and Reposition postures, while one postural style was chosen for Turn Away and Turn Toward. The two styles for Lie-to-Sit and Reposition involved a push or a pull technique, while the Sit-to-Chair technique was completed at two different bed heights. The posture in which peak force application occurred was based on these techniques, and this posture was modeled in 3DSSPP, as well as the five recommended techniques [29]. Average height and weight of the 20 participants was used as anthropometric input for all techniques modeled in 3DSSPP. Analysis of these positions consisted of dividing the given required moment by the population mean strengths for both the untrained techniques and trained techniques to generate a required strength fraction.

2.6. Statistical analysis

All statistical analyses were performed using JMP 8.0 software (SAS Institute, North Carolina, USA). Statistical significance was set at $\alpha = 0.05$ for all scenarios, with Student’s T-Test post-hoc testing where appropriate. One way ANOVAs were completed separately for each of the five tasks using peak moment for the right shoulder, left shoulder and low back as dependent variables, with training state as the independent factor. The magnitude of change between pre- and post-training state on these peak moments was also expressed as a percentage change.

3. Results

Training had differential responses on shoulder and low back loading and strength requirements, and typically resulted in decreased low back loading and variable responses at the shoulder. Required strength fractions generally decreased at the low back, but was variable at the shoulder (Table 1). The results are divided by task in the following sections.

3.1. Lie-to-Sit

Training decreased peak moments in the low back and right shoulder, but not the left shoulder. The peak resultant low back moment decreased by 42% ($p < 0.01$) (Table 2). The left and right shoulders decreased by 26% ($p < 0.01$) and 1%, respectively ($p = 0.96$). Mean population strength fractions were decreased with technique changes following training in the left shoulder, right shoulder and low back by 36%, 42%, and 33%, respectively. However, the post-training technique increased right shoulder population strength fractions by 101%, decreased the left shoulder by 38%, and increased the low back by 12% compared to the untrained push technique.

3.2. Reposition

Training decreased low back, but not shoulder peak moments. Low back peak moments decreased by 43% ($p < 0.01$), while the shoulders had non-significant results. Trained trials in the reposition task increased right shoulder peak moment loading by 15% ($p = 0.26$), while decreasing the left shoulder by 19% ($p = 0.10$). For mean population strength fractions, trained techniques compared to untrained pulls exertions had increased right shoulder and low back strength fractions, while decreasing or maintaining left shoulder strength fractions (Table 1).
Comparisons of mean population strength required for self-selected MPH techniques versus recommended MPH techniques. Percentages in Untrained and Trained rows represent percentage of mean population strength.

<table>
<thead>
<tr>
<th>TASK</th>
<th>Condition</th>
<th>Right shoulder</th>
<th>Left shoulder</th>
<th>Low back</th>
</tr>
</thead>
<tbody>
<tr>
<td>Lie-to-Sit</td>
<td>Untrained (Pull)</td>
<td>215%</td>
<td>171%</td>
<td>199%</td>
</tr>
<tr>
<td></td>
<td>Untrained (Push)</td>
<td>68%</td>
<td>160%</td>
<td>118%</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>136%</td>
<td>99%</td>
<td>132%</td>
</tr>
<tr>
<td></td>
<td>% Change (Pull)</td>
<td>−36%</td>
<td>−42%</td>
<td>−33%</td>
</tr>
<tr>
<td></td>
<td>% Change (Push)</td>
<td>+101%</td>
<td>−38%</td>
<td>+12%</td>
</tr>
<tr>
<td>Reposition</td>
<td>Untrained (High Bed)</td>
<td>151%</td>
<td>157%</td>
<td>175%</td>
</tr>
<tr>
<td></td>
<td>Untrained (Low Bed)</td>
<td>140%</td>
<td>179%</td>
<td>149%</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>169%</td>
<td>157%</td>
<td>182%</td>
</tr>
<tr>
<td></td>
<td>% Change (High Bed)</td>
<td>+12%</td>
<td>0%</td>
<td>+4%</td>
</tr>
<tr>
<td></td>
<td>% Change (Low Bed)</td>
<td>+20%</td>
<td>−13%</td>
<td>+3%</td>
</tr>
<tr>
<td>Sit-to-Chair</td>
<td>Untrained (Pull)</td>
<td>58%</td>
<td>45%</td>
<td>53%</td>
</tr>
<tr>
<td></td>
<td>Untrained (Push)</td>
<td>70%</td>
<td>89%</td>
<td>50%</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>109%</td>
<td>88%</td>
<td>56%</td>
</tr>
<tr>
<td></td>
<td>% Change (Pull)</td>
<td>+89%</td>
<td>+94%</td>
<td>+5%</td>
</tr>
<tr>
<td></td>
<td>% Change (Push)</td>
<td>+56%</td>
<td>−1%</td>
<td>+11%</td>
</tr>
<tr>
<td>Turn Away</td>
<td>Untrained</td>
<td>119%</td>
<td>140%</td>
<td>68%</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>101%</td>
<td>88%</td>
<td>32%</td>
</tr>
<tr>
<td></td>
<td>% Change</td>
<td>−15%</td>
<td>−38%</td>
<td>−53%</td>
</tr>
<tr>
<td>Turn toward</td>
<td>Untrained</td>
<td>70%</td>
<td>85%</td>
<td>73%</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>94%</td>
<td>102%</td>
<td>35%</td>
</tr>
<tr>
<td></td>
<td>% Change</td>
<td>+35%</td>
<td>+19%</td>
<td>−52%</td>
</tr>
</tbody>
</table>

Peak joint moments (in Nm) during self-selected and trained MPH techniques. Significant differences between untrained and trained conditions within regions are bold.

<table>
<thead>
<tr>
<th>TASK</th>
<th>Condition</th>
<th>Right shoulder</th>
<th>Left shoulder</th>
<th>Low back</th>
</tr>
</thead>
<tbody>
<tr>
<td>Lie-to-Sit</td>
<td>Untrained</td>
<td>47.2</td>
<td>61.3</td>
<td>231.8</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>46.9</td>
<td>45.3</td>
<td>133.5</td>
</tr>
<tr>
<td>Reposition</td>
<td>Untrained</td>
<td>50.6</td>
<td>62.8</td>
<td>195.1</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>58.3</td>
<td>50.6</td>
<td>109.5</td>
</tr>
<tr>
<td>Sit-to-Chair</td>
<td>Untrained</td>
<td>27.3</td>
<td>29.3</td>
<td>197.0</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>56.7</td>
<td>57.7</td>
<td>153.5</td>
</tr>
<tr>
<td>Turn away</td>
<td>Untrained</td>
<td>41.7</td>
<td>41.2</td>
<td>206.8</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>35.7</td>
<td>36.6</td>
<td>114.7</td>
</tr>
<tr>
<td>Toward</td>
<td>Untrained</td>
<td>49.6</td>
<td>65.1</td>
<td>145.7</td>
</tr>
<tr>
<td></td>
<td>Trained</td>
<td>46.1</td>
<td>53.0</td>
<td>112.0</td>
</tr>
</tbody>
</table>

3.3. **Sit-to-Chair**

Training generated increases in peak moments in both shoulders, but decreases at the low back. Peak moments in the left shoulder and right shoulder increased during trained exertions by 97% and 107% respectively ($p < 0.01$). The low back peak moment decreased by 45 Nm ($p = 0.03$). The recommended technique compared to the untrained techniques increased right shoulder strength fractions and had variable effects on the left shoulder and low back (Table 1).

3.4. **Turn away**

Low back peak moments decreased following training, but no changes existed in the shoulders. The low back moment decreased by 92 Nm ($p < 0.01$), a 44% decrease. Moments in the left and right
Fig. 2. Joint specific peak resultant moments for the Sit-to-Chair task when considering training state as an independent factor. Significant differences between pre- and post-training are marked by an asterisk.

Fig. 3. Joint specific peak resultant moments and percentage of mean population strength for the Turn Toward task. Significant differences between joint specific peak resultant moments between pre- and post-training are marked by an asterisk. Columns are for peak resultant moments (PM in legend), lines are for percentage of mean population joint strength (JS in legend).

3.5. Turn toward

Decreases existed in the left shoulder and the low back, but not the right shoulder. The left shoulder moment decreased by 12.1 Nm or 18% ($p = 0.03$), while the low back decreased by 33 Nm ($p < 0.01$), a 23% change. The right shoulder decreased insignificantly by 7% ($p = 0.43$). Trained exertions increased mean population strength fractions required in the shoulders (35% for the right, 19% for the left), but decreased the low back by 52%.

4. Discussion

The focus of this research was to examine if techniques designed to decrease low back demands transferred these exposures to the shoulders, or if overall loading decreased holistically. Peak resultant
magnitudes were reduced for the low back for every task, and reductions occurred for the shoulders in some tasks, but demands increased after training for others, indicating a spectrum of exposures. Peak moments at the low back decreased by 22–44%, depending on the task. This confirms previous reports of decreased low back exposures with recommended manual patient handling techniques [9,24,30]. Peak resultant moments at the right shoulder increased using the recommended techniques for two of the five tasks, with no change in a third task and increases in two tasks; left shoulder peak moments decreased in four of five scenarios. The identified moment increases suggest possible exposure transfers from the low back to the shoulder.

These changes were then converted into a common scale by replicating the postures assumed by the participants during peak force exertion were within a static strength analysis program (3DSSPP) and interpreted. This provided an estimate of how capable the study population is of performing the techniques compared to population normative strength data [29]. For several tasks, the required strength at the shoulders and low back exceeded the mean population strength while using the recommended techniques, increasing overexertion risk [31,32]. In many cases, using the recommended techniques increased the percentage of mean population strength required to complete the tasks at the shoulders. The recommended techniques required at least 88% of the mean population strength at both shoulders for all tasks, and every scenario except Turn Away resulted in increased strength requirements compared to novice techniques in at least one shoulder.

Joint demand loading changes are readily identified in the Turn Toward and Sit-to-Chair tasks. In the Turn Toward task, the untrained technique balanced exposures nearly equally amongst all three joints, with each joint requiring approximately 75% of the mean population joint strength. Once the recommended technique was adopted, the low back mean population strength fraction decreased to 35%, while the left and right shoulders increased to nearly 100% mean joint strength fraction. This confirms previous recognition of the Turn Toward task as a stressful nursing task [33]. The largest increase occurred in the Sit-to-Chair task, with peak resultant moments at the right and left shoulders increasing by 107% and 97%, respectively, while the low back moment decreased by 22%. This task is frequently targeted for replacement with mechanical lift assists [34]. The strength requirement changes establish both the overall high demand of these MPH tasks while highlighting the potential for transfer of demand between joints for certain tasks.

Field examination of manual patient handling is challenging due to complex interaction between nurse and patient in various situations, and this generated limitations in our work. At present, there is no benchmark for recording separate hand forces in manual patient handling scenarios [35,36]. The current research did not want to interfere with participant techniques or generate compensations through encumbrance of heavy or awkward equipment, and hand demands (such as holding dynamometers during transfers) are known to affect strategies [37,38]. Absolute direction of the force applied was estimated, and the use of this method limits analysis to calculation of peak moments, potentially over- or underestimating peak joint moments. However, this study was primarily interested in changes related to training and task type and relative rather than absolute magnitudes. The estimated magnitudes were of similar shoulder moment magnitudes for previous reposition tasks, confirming the reasonableness of the approach [19]. Finally, the set of manual patient handling tasks was not exhaustive, and each participant was limited to approaching the left side of the bed. Approaching from the opposite side of the bed may have generated bilaterally opposite exposures, but anecdotal evidence from practicing nurses suggests that handedness is not typically considered in manual patient handling.
5. Conclusion

This study supports a recommended of continued implementation of several of the manual patient handling techniques; however, certain cautions should be considered for some transfers. The recommended techniques were aimed specifically at lowering low back injury exposures, but may transferring demands to the shoulders. The Turn Toward and Sit-to-Chair tasks appear to adversely affect the shoulder the most, suggesting they should be avoided if possible. Future investigations may benefit from developing novel holistic patient handling techniques that do not transfer demands to other areas of the body.

Conflict of interest

The authors have no conflict of interest to report.

References


