

Melatonin Effects on EEG Activity During Sleep Onset in Mild-to-Moderate Alzheimer's Disease: A Pilot Study

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Abstract. There is evidence demonstrating that 5-mg of fast-release melatonin significantly reduces nocturnal sleep onset in patients with mild-to-moderate Alzheimer's disease (AD). However, the physiological mechanism that could promote sleep installation by melatonin in patients with AD is still poorly understood. The present pilot study was designed to analyze the effects of melatonin on cortical activity during the sleep onset period (SOP) in eight mild-to-moderate AD patients treated with 5-mg of fast-release melatonin. Electroencephalographic recordings were obtained from C3-A1, C4-A2, F7-T3, F8-T4, F3-F4, and O1-O2. The relative power (RP), interhemispheric, intrahemispheric, and fronto-posterior correlations of six electroencephalographic bands were calculated and compared between two conditions: placebo and melatonin. Results show that at F7-T3, F3-F4, and C3-A1, melatonin induced an increase of the RP of the delta band. Likewise, in F7-T3, melatonin induced a decrease of the RP in the alpha1 band. Similarly, results show a lower interhemispheric correlation between the F7-T3 and F8-T4 derivations in the alpha1 band compared to the placebo condition. We conclude that the short sleep onset related to melatonin intake in AD patients was associated with a lower RP of the alpha1, a higher RP of the delta band (mainly in the left hemisphere) and a decreased interhemispheric EEG coupling in the alpha1 band. The possible role of the GABAergic neurotransmission as well as of the cascade of neurochemical events that melatonin triggers on sleep onset are discussed.

Keywords: Alzheimer's disease, EEG correlation, electroencephalography, melatonin, relative power, sleep onset, suprachiasmatic nucleus

INTRODUCTION

Although difficulty in falling asleep during the night is a common symptom of Alzheimer's disease

(AD) [1–6], few studies have focused on testing pharmacological alternatives for treating sleep-related problems in AD patients [7]. One well-known treatment for sleep disturbances is melatonin (N-acetyl-5-methoxytryptamine), which plays a major role in regulating circadian rhythms. Melatonin is a hormone secreted by the pineal gland that modulates the sleep-wake cycle. Its secretion is enhanced during darkness and suppressed during day light [8].

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In healthy subjects, melatonin has been shown to decrease sleep onset latency, increase total sleep time, and improve overall sleep quality [9]. Regarding neural activity, there is evidence that after melatonin administration the electroencephalographic activity (EEG) of healthy subject's exhibits increased sleep spindles but reduced slow-wave activity [10]. In a previous study, we demonstrated that 5 mg of fast-release melatonin significantly reduced nocturnal sleep onset in patients with mild-to-moderate AD [11]. This reduction of sleep onset approaches the values reported for non-dementia geriatric patients [12]. However, the physiological mechanism through which melatonin promotes sleep installation is still only poorly understood.

The locations and pharmacology of melatonin receptors have been reviewed extensively. Two cloned receptors, MT₁ and MT₂, are of particular importance for rhythm physiology and pharmacology [13, 14]. Using gene knockout technology in mice and pharmacological manipulations, Liu et al. [15] found that the phase-shifting melatonin receptor in the suprachiasmatic nucleus (SCN) is MT₂, while MT₁ is associated with acute suppression of electrical activity in the SCN. In fact, there is evidence that MT₁ receptors expressed in cell preparations [16, 17] activate Kir3 channels that underlie melatonin-induced increases in potassium conductance that, in turn, enhance GABAergic activity [18]. It has been shown that GABAergic cells in the hypothalamus, basal forebrain (BF), and the median (mPO) and ventrolateral preoptic areas (VLPO) are highly-active during sleep onset [19–22]. In addition, EEG activity observed during sleep onset has been related to GABAergic modulation in the hypothalamus, BF, mPO, and VLPO areas [23, 24].

Quantitative EEG analyses in healthy adult subjects have shown that the sleep onset period (SOP) is characterized by smooth changes during which the power of the fast frequencies decreases, while that of the low frequencies gradually increases [25–28]. Also, the degree of synchronization between EEG signals has been used to determine the functional relation between cortical areas associated with normal SOP. Morikawa et al. found that delta band synchronization between occipital and frontal regions and between central and parietal areas dropped sharply just before the alpha band disappeared during SOP [29]. Those authors further reported decreases in alpha synchronization 2-3 min before SOP, and detected significant increases in the synchronization of the fast frequencies just before the installation

of stage 2 of non-rapid eye movement sleep (N-REM2) [30]. Likewise, a significant decrease in fronto-occipital and inter-frontal synchronization in the alpha band has been observed during SOP [31]. Finally, Kikuchi et al. conducted a study to examine interhemispheric EEG synchronization during the state of rest in elderly subjects, finding low EEG synchronization for the delta, theta, alpha and beta bands [32].

Considering that SOP is characterized by a specific EEG pattern in both elderly and healthy adult subjects, and that 5-mg of fast-release melatonin reduces latency to sleep onset in AD patients [11], the aim of the present study was to determine the effect of melatonin on EEG activity and the degree of EEG synchronization between different cortical areas in AD patients. We hypothesized that the facilitator effect of melatonin on SOP in AD patients will be associated with the generation of slow frequencies (delta, theta and alpha bands), together with a decrease in the activity of the fast frequencies (beta band) during SOP. Likewise, we proposed that melatonin will reduce the intrahemispheric, interhemispheric, and fronto-anterior correlation of the alpha band, while increasing the delta band correlation, compared to the placebo condition. To test these hypotheses, we evaluated the effects of melatonin during SOP on EEG spectral power and on intrahemispheric, interhemispheric, and fronto-anterior correlations in AD patients previously treated with melatonin [11].

MATERIALS AND METHODS

Participants

Eight patients with mild-to-moderate AD were recruited for this study. Their mean age was 65 years [\pm SE: 2.32]. Diagnoses of AD were conducted with neurological testing that clinically established the dementia syndrome. In an effort to obtain diagnoses of reversible dementia, the following tests were performed, following the suggestions of Barry et al. [33] and Amodar et al. [34]: blood count, blood chemistry, thyroid and hepatic function, simple contrasted CAT scan, and assessment of ischemic factors using the Helsinki scale. Also, an EEG study was conducted to discard epilepsy. The diagnostic criteria applied were adapted from those published by the National Institute of Neurological and Communicative Disorders and Stroke/Alzheimer's Disease and

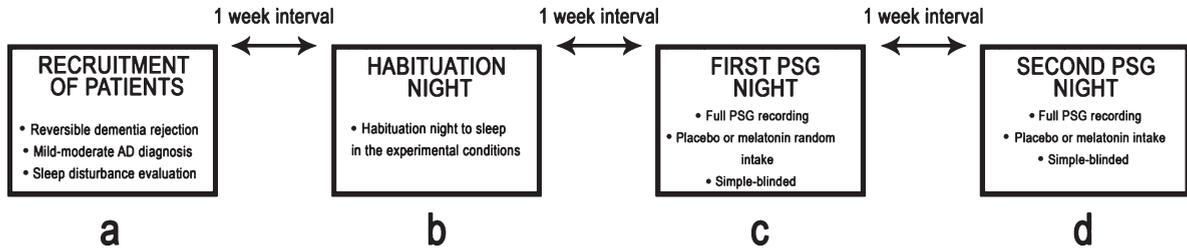


Fig. 1. Schematic representation of the experimental design.

Related Disorders Association (NINCDS-ADRDA) Work Group [35]. Global dementia severity was classified in accordance with the Clinical Dementia Rating (CDR) scale [36], where 0 indicates no cognitive impairment and 0.5, 1, 2, and 3 indicate very mild, mild, moderate, and severe dementia, respectively. One inclusion criterion was that subjects were considered to be suffering from mild-to-moderate AD; a second was alterations in sleep onset, which were evaluated in a clinical interview designed in our laboratory and applied to the caregiver who spends the night with each subject.

Informed consent was obtained from patients and their relatives or caregivers through the Outpatient Department. This study was approved by the Ethics Committee on Human Research of the National Institute of Psychiatry “Ramón de la Fuente Muñiz” (Project: NC093340.2) and complied with the guidelines established by the National Institutes of Health in the USA. Moreover, the work was carried out in strict accordance with The Code of Ethics of the World Medical Association (Helsinki Declaration, 1975) for experiments involving humans. It is important to note that none of the patients had received previous pharmacological treatment based on acetylcholine inhibitors or any other medication prescribed for dementia. Likewise, none had received prior pharmacological treatment for sleep disturbances or any other medication that could impact sleep.

Procedures

A single-blind, placebo-controlled study was conducted. A total of three nights of PSG recordings were obtained from each patient. The first night was considered a habituation session. On the second night, either an oral placebo or a 5-mg dose of fast-release melatonin (BIOQUIMED Labs) was administered, and full PSG recording was performed. On the third

night, either an oral placebo or a 5-mg dose of fast-release melatonin was administered with full PSG recording. Both the melatonin and placebo were administered one hour before PSG recording began (approximately at 9:00 p.m.). The order of treatments was counterbalanced. When recording ended, and the study finalized, the patients withdrew from the laboratory. The three recordings were carried out within a one-week interval. Figure 1 illustrates our experimental design.

PSG recordings

Electrodes were placed at bipolar, F7-T3, F8-T4, F3-F4, O1-O2 and referential, C3-A1, C4-A2, derivations in accordance with the 10–20 international system for human EEG recording [37]. Two electrodes were attached superficially to both ocular canthi to obtain electrooculograms (EOG), while two additional electrodes were attached to the mentalis muscle to obtain electromyograms (EMG). All PSG recordings were performed during 9 h, from 10:00 p.m. to 7:00 a.m., in a room specially-designed for PSG studies, equipped with adequate audio and video monitoring systems. PSG signals were acquired with a Grass Model 15 polygraph and model 15A4 amplifiers (Grass-Telefactor, West Warwick, RI, USA). The sampling rate was set at 512 Hz, the high-pass at 1 Hz and the low-pass filter frequencies at 70 Hz.

Data analysis

SOP was scored, analyzed and then assessed visually in 20-s epochs. These periods consisted of transitional episodes from wakefulness to N-REM1 sleep. For the digital analyses, we chose a 6-min sample of EEG from the wake-sleep transition, the last 3 min of wakefulness, and the first 3 min of N-REM1 sleep, similar to the report of Hori’s H2-H3 states of wake-sleep transition [38]. The PSG patterns

of wakefulness and N-REM1 were evaluated using international standards for visual evaluation of PSG recordings in humans [39]. Sleep latency, defined as the time that elapsed from lights off to onset of N-REM1, was also evaluated. All PSG recordings were made using GAMMA software (Grass, Co).

For digital EEG analyses, the EEG signals from the last 3 min of wakefulness and the first 3 min of N-REM1 sleep were examined off-line with CHECAsEN software [40] to remove recordings altered by electrical EOG and EMG artifacts. The CHECAsEN programs permits off-line, visual inspection of previously digitized electroencephalographic signals to eliminate segments contaminated by artifacts (for details about the software see: <http://www.medigraphic.com/pdfs/inge/ib-2010/ib102g.pdf>). By means of the CHECAsEN software, a total of 634 non-artifact-free segments of wakefulness and 610 non-artifact-free segments of N-REM1 were rejected ($n=8$). Thus, a total of 180 artifact-free, 1-s EEG segments (90 of wakefulness and 90 of N-REM1 sleep) from each subject and condition (placebo, melatonin) were analyzed using EEGmagic software to obtain the relative power (RP) of the EEG bands (i.e., the proportional contribution of each band expressed as a percentage of total power), and the functional synchronization between successive amplitude values of EEG segments in the EEG derivations [41]. EEGmagic first applies the Fast Fourier Transform to the EEG signals to obtain the RP values of frequencies grouped in broad bands. For purposes of the present study, the frequency bands were established as follows: delta (1–3.0 Hz), theta (4–7.0 Hz), alpha1 (8–10.0 Hz), alpha2 (11–13.0 Hz), beta1 (14–19.0 Hz), and beta2 (20–30 Hz). The parameters analyzed with EEGmagic were calculated following the steps indicated in Fig. 2. The instantaneous spectrum of the digitized signals was obtained by calculating the real and imaginary parts of the direct discrete Fourier transform using formulas 1–3 (Fig. 3a). Formulas 4–13 were applied to calculate the auto-spectra (average) and crossed spectrum (average) of the digitized signals (Fig. 3b). Later, formula 14 was applied by the EEGmagic program to calculate the Pearson product-moment correlation coefficients (r) (Fig. 3c) between bilateral regions (interhemispheric correlation: C3-A1 with C4-A2, and F7-T3 with F8-T4), between regions in the same hemisphere (intrahemispheric correlation: C3-A1 with F7-T3 and C4-A2 with F8-T4), and between fronto-posterior regions (F3-F4 with O1-O2).

Statistical analyses

Sleep latencies under the placebo and melatonin conditions were assessed using two correlated-groups Student t tests with significance set at $p \leq 0.05$. For RP and r analyses, the EEG bands were also assessed using correlated-groups Student t tests with significance set at $p \leq 0.05$. For statistical purposes, r values were transformed to Fisher's z -scores and RP values were transformed to natural logarithms.

RESULTS

Sociodemographic and sleep data

The sociodemographic information and sleep characteristics of the eight patients with mild-to-moderate AD are shown in Table 1. Their mean age was 65.62 years ($SE \pm 1.01$) and mean education level was 9.37 years ($SE \pm 1.05$). Only one was living alone at the time of study. Diagnoses determined that 50% of these patients had mild AD and that the other 50% had moderate AD. The most common sleep disturbance reported was insomnia. The sleep latency of the patients in the placebo condition had a mean of 34.75 min ($SE \pm 8.54$), but after melatonin administration this decreased significantly (mean = 15.25 min, $SE \pm 2.10$) ($t=2.21$, $df=14$, $p=0.04$).

Relative power

After melatonin administration, a significant increase of RP in delta ($t=-5.49$, $df=7$, $p=0.0009$) with a decrease in alpha1 ($t=5.048$, $df=7$, $p=0.0014$) were observed at F7-T3 compared to the placebo group (Fig. 4b). Likewise, after melatonin administration, a significant increase of RP in delta ($t=-2.54$, $df=7$, $p=0.03$) was observed at F3-F4 compared to the placebo group (Fig. 4c). At C3-A1, an important increase of RP in delta ($t=-2.495$, $df=7$, $p=0.04$) was obtained compared to the placebo group (Fig. 4d). No significant differences were observed at the O1-O2 derivations, nor were significant changes in the RP of the EEG bands seen after melatonin administration in the right hemisphere compared to the placebo group.

Interhemispheric correlation

As Fig. 5 shows, the degree of EEG coupling between the F7-T3 and F8-T4 derivations was lower

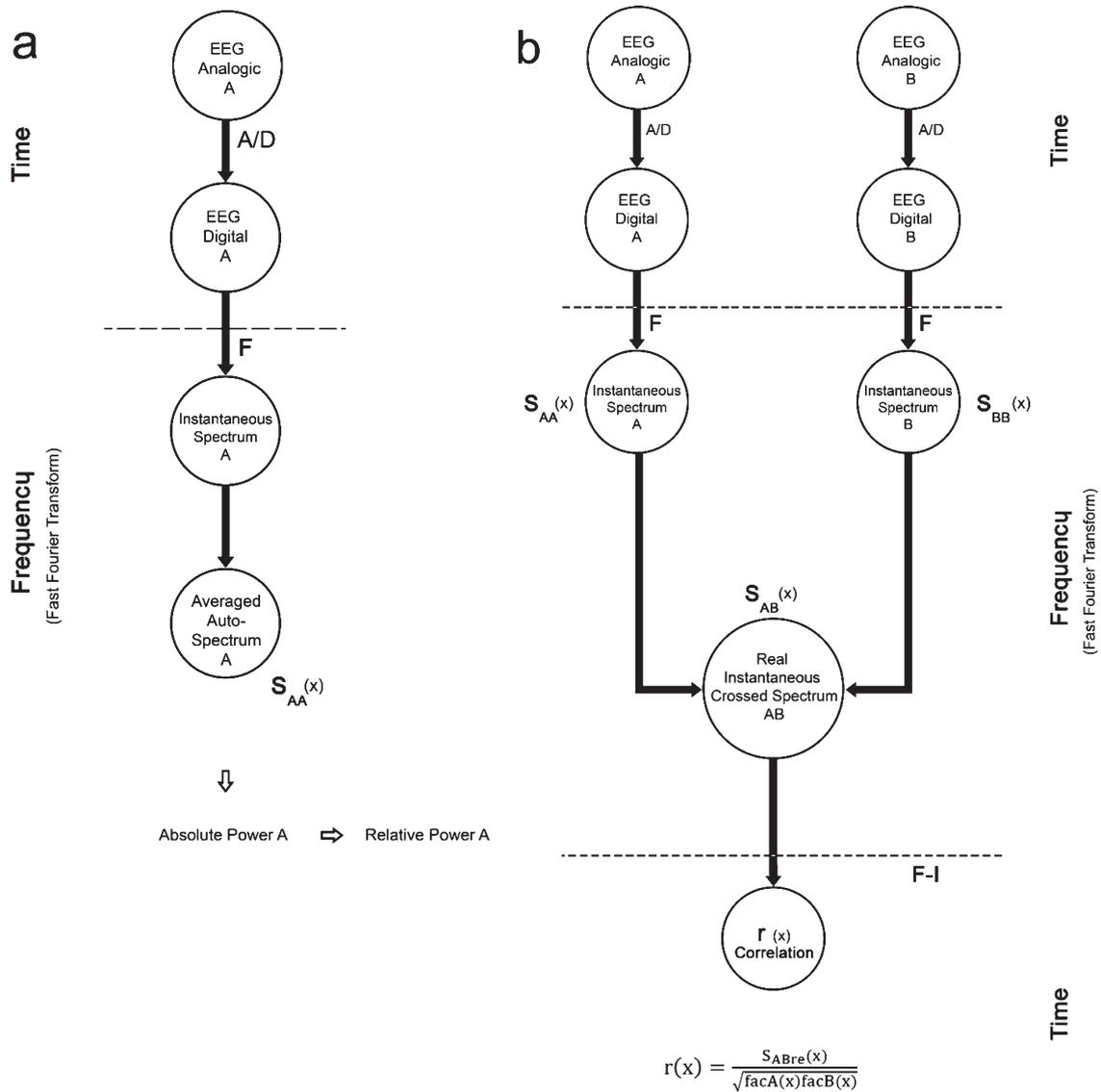


Fig. 2. Method used to calculate the relative power spectra and correlation: (a) the analog signals A and B are digitized and then used to obtain the instantaneous spectra of each signal; (b) subsequently, the autospectra (SAA and SBB) and crossed spectrum (SAB) are calculated. The cross-correlation function is obtained with the Fourier Inverse Transform (F-I) of the crossed spectrum.

in the alpha1 band in patients treated with melatonin ($t = 2.39$, $df = 7$, $p = 0.04$) than in those who received the placebo. No differences were found when the intrahemispheric and fronto-posterior correlations between the placebo and melatonin conditions were compared.

DISCUSSION

To the best of our knowledge, this is the first study to analyze the effect of melatonin on EEG activity and its relation to the installation of sleep in AD patients.

In general, melatonin administration induced EEGs similar to those observed in healthy subjects in our AD patients during SOP [25–27,42–44]; i.e., a significant increase of RP in the slow frequencies (mainly delta) with a decrease of RP in the alpha band. However, there is evidence that the most representative change in SOP in healthy subjects is the predominance of slow-wave activity in the prefrontal cortex [45]. In this regard, our results showed a significant increase in the delta band at C3-A1 and F7-T3 during SOP that was related to melatonin administration. Likewise, we observed an increase in the RP of the

a

$$\text{Fre}(x) = \sum_{n=0}^{N-1} f(n) \cos\left(\frac{2\pi nx}{N}\right) \quad (1)$$

$$\text{Fim}(x) = - \sum_{n=0}^{N-1} f(n) \text{sen}\left(\frac{2\pi nx}{N}\right) \quad (2)$$

$$\text{Pot}(x) = \{\text{Fre}(x)\}^2 + \{\text{Fim}(x)\}^2 \quad (3)$$

Where:

f(n), n=0,1,2,...,N-1 N points of the signal segment in time.

Fre(x), x=0,1,2,...,N-1 the N values of the real part of the signal spectrum f(n).

Fim(x), x=0,1,2,...,N-1 values of the imaginary part of the signal spectrum f(n).

Pot(x), x=0,1,2,...,N-1 N power auto spectrum values of the signal f(n).

b

$$S_{AA}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} A_i^*(x) A_i(x) \quad (4)$$

$$S_{AA}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} \{(\text{FreA}(x) - \text{FimA}(x)) (\text{FreA}(x) + \text{FimA}(x))\} \quad (5)$$

$$S_{AA}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} \{((\text{FreA}(x))^2 + ((\text{FimA}(x))^2)\} \quad (6)$$

$$S_{BB}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} B_i^*(x) B_i(x) \quad (7)$$

$$S_{BB}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} \{(\text{FreB}(x) - \text{FimB}(x)) (\text{FreB}(x) + \text{FimB}(x))\} \quad (8)$$

$$S_{BB}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} \{((\text{FreB}(x))^2 + ((\text{FimB}(x))^2)\} \quad (9)$$

$$S_{AB}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} A_i^*(x) B_i(x) \quad (10)$$

$$S_{AB}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} \{(\text{FreA}(x) - \text{FimA}(x)) (\text{FreB}(x) + \text{FimB}(x))\} \quad (11)$$

$$S_{ABre}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} \{(\text{FreA}(x)\text{FreB}(x)) + (\text{FimA}(x)\text{FimB}(x))\} \quad (12)$$

$$S_{ABim}(x) = \lim_{nd \rightarrow \infty} \left(\frac{1}{nd}\right) \sum_{i=1}^{nd} \{(\text{FreA}(x)\text{FimB}(x)) - (\text{FimA}(x)\text{FreB}(x))\} \quad (13)$$

Where:

nd = number of segments

Ai (x), Bi (x) = instantaneous spectra of signals A and B at frequency x

Ai * (x), Bi * (x) = conjugates of the instantaneous spectra of signals

A and B at frequency x (the conjugate of a complex number is obtained by inverting the sign of the imaginary part)

C

$$r(x) = \frac{S_{ABre}(x)}{\sqrt{\text{facA}(x)\text{facB}(x)}} \quad (14)$$

Where facA and facB are defined by the formulas:

$$\text{facA}(x) = \frac{1}{N} \sum_{x=0}^{N-1} \text{FreA}(x) \quad (15)$$

$$\text{facB}(x) = \frac{1}{N} \sum_{x=0}^{N-1} \text{FreB}(x) \quad (16)$$

Fig. 3. Formulas used to calculate the power spectra (a, b,) and the electroencephalographic correlation (c).

Table 1
Sociodemographic and sleep characteristics of eight patients with mild-to-moderate Alzheimer's disease

	Age (y)	Education (y)	Living arrangements	CDR evaluation	Sleep disturbances	Sleep latency (min)	
						Placebo	Melatonin*
Patient1	65	9	Wife and others	Moderate	Insomnia/sleep bruxism	45.5	15.0
Patient2	61	15	Wife only	Mild	Insomnia/periodic limb movement	11.5	13.0
Patient3	65	10	Other relatives	Moderate	Insomnia	37.0	14.0
Patient4	69	6	Alone	Moderate	Insomnia/parasomnia	80.0	9.0
Patient5	69	7	Others	Mild	Insomnia/sleep bruxism	42.0	8.5
Patient6	63	12	Others	Mild	Insomnia	16.5	27.0
Patient7	68	7	Wife and others	Moderate	Insomnia/periodic limb movement	4.0	16.0
Patient8	65	9	Wife and others	Mild	Insomnia	41.5	19.5
	Mean = 65,62	Mean = 9,37				Mean = 34,75	Mean = 15,25
	SE ± 1.017	SE ± 1.05				SE ± 8.54	SE ± 2.10
							*($t = 2.21$, $df = 14$, $p = 0.04$)

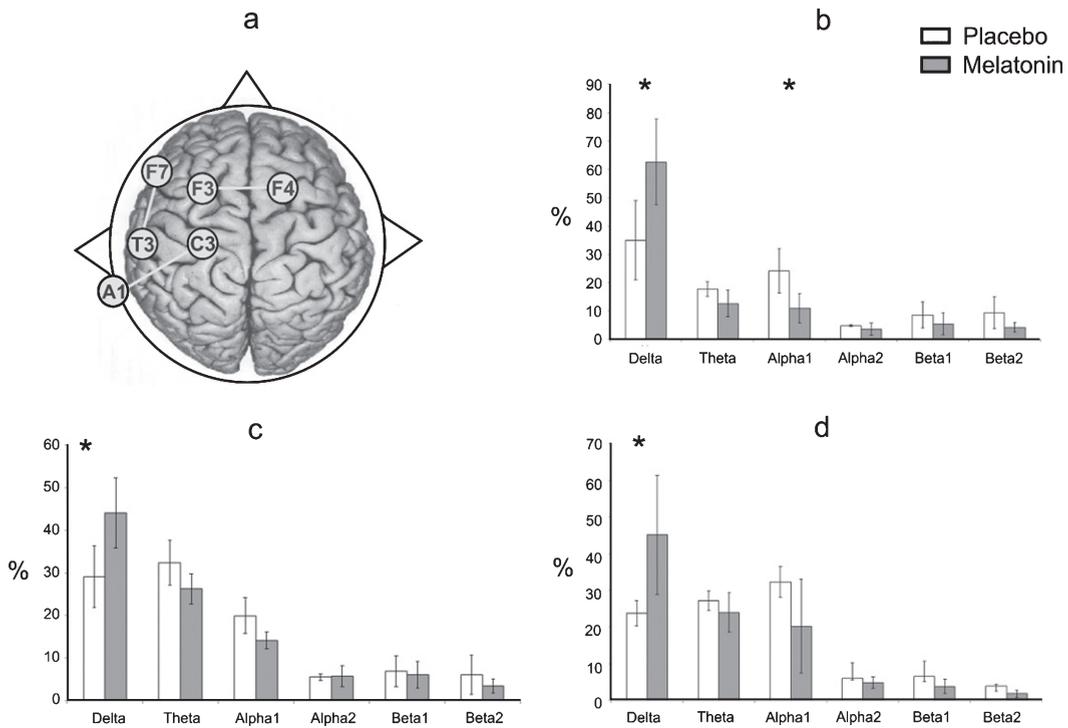


Fig. 4. a) This diagram represents the EEG derivations in which significant differences were obtained. Relative power (in %) of the EEG bands recorded at F7-T3 (b), F3-F4 (c) and C3-A1 (d) of the EEG derivations during the wake-sleep transition in the placebo (white bars) and melatonin (gray bars) conditions. Results are shown as mean ± 2SE. Asterisks indicate significant differences with $*p \leq 0.05$.

delta band after melatonin administration at F3-F4. These results suggest that the predominance of slow waves in the prefrontal cortex is necessary for an optimal transition from wakefulness to sleep, and that this can be facilitated by administering melatonin to AD patients.

In addition to EEG power, our study analyzed the degree of correlation between the EEG signals from

different cortical areas, with the result that characteristic degrees of cortical correlation in the different conditions were found. The degree of interhemispheric correlation between the F7-T3 and F8-T4 derivations in the alpha1 band was lower after melatonin administration than in the placebo condition. This result supports our hypothesis and concurs with various other studies which have reported that EEG

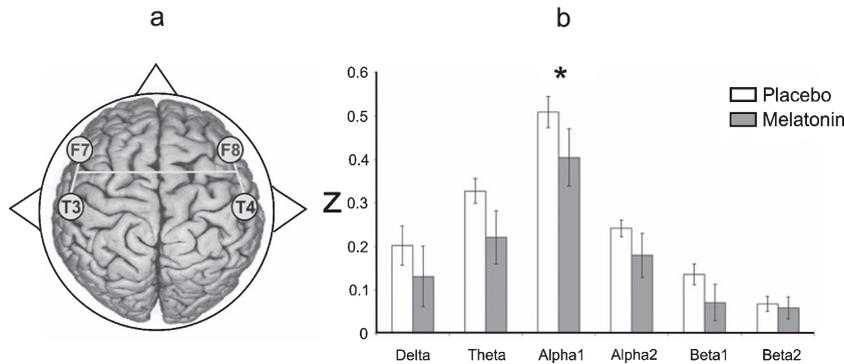


Fig. 5. a) Representative diagram of the EEG derivations in which significant differences were obtained. b) Interhemispheric correlation (in z-values) of the EEG bands recorded between F7-T3 and F8-T4 during the wake-sleep transition after administering placebo (white bars) and melatonin (gray bars). Results are shown as mean \pm 2SE. Asterisks indicate significant differences with $*p \leq 0.05$.

synchronization during SOP in healthy subjects is associated with decreased correlation in the alpha band [28, 30–32].

There is evidence that the extension of synchronizing signals from associative prefrontal to posterior areas plays a role in the wake-to-sleep transition [46]. Topographic maps of coherence in delta-to-theta band activity have demonstrated that the synchronous component at the anterior-central areas of the scalp appears to correspond to increasing power [47]. Likewise, a prevalence of an occipital-to-frontal information flow in the delta, theta and alpha bands during the pre-sleep period, and a prevalence of a frontal-to-parieto-occipital information flow in all bands during SOP have been demonstrated in healthy subjects [48]. However, we did not observe a higher degree of EEG coupling between the F3-F4 and O1-O2 derivations after melatonin administration. Although the precise mechanism underlying these coherence abnormalities is unclear, it has been suggested that as the inter-neuronal distance for information propagation increases coherence is lowered, since AD shows diffuse and widespread cerebral degenerations [49, 50]. These studies suggest that a decrease in EEG correlation is associated with the presence of periventricular white matter lesions, which can cause functional disconnections between brain regions. Since neuroimaging studies have shown that periventricular white matter lesions, or leukoaraiosis, are observed more frequently in AD patients than in control subjects [51, 52], changes such as these may be another factor that reduces functional connectivity in AD patients.

As mentioned above, there is evidence to support the idea that melatonin induces sleep by modulating GABAA receptors [53–56]. Indeed, study data have

shown that GABAergic cells of the hypothalamus, BF, mPO, and VLPO in the hypothalamic area are highly-active during sleep onset [19–22]. Moreover, it has been demonstrated that EEG activity observed during sleep onset is related to GABAergic activity in these structures [24, 57–65]. Hence, it is probable that the beneficial effect of melatonin (i.e., decreased sleep latency) on sleep onset in AD patients could be associated with a functioning of the GABAergic system that was sufficient to generate an EEG pattern similar to those manifested by healthy subjects during normal sleep onset. AD is associated with a broad loss of synapse density and the continuous degeneration of cholinergic and glutamatergic pathways [66]. Although the occurrence of disruptions of excitatory pathways is widely-recognized, inhibitory GABAergic pathways are generally thought to be well-preserved in AD [67, 68].

The present study found a reduction of sleep onset latencies, noting that they approached the normal time previously reported for geriatric non-dementia patients [12]. In fact, the effect of rapid installation of sleep after melatonin administration in non-dementia geriatric patients has been documented previously through observations which found that 3 mg of this indolamine facilitate the rapid installation of non-REM sleep [69], as was observed in our study. These results could suggest that, even in patients with mild-to-moderate AD, the brain structures involved in sleep control and regulation (such as the suprachiasmatic nucleus, thalamic-cortical circuits and the brain stem), are capable of reacting to the cascade of events that melatonin triggers to facilitate sleep installation. Our results show that in three patients, SOP was unexpectedly prolonged after melatonin as compared to placebo. This unforeseen finding

suggests that in some patients with mild-to-moderate AD, the brain structures involved in sleep control and regulation may be affected by AD neurodegeneration.

Study limitations

It is important to note that the present work has some methodological limitations intrinsic to a pilot study, such as the lack of a control group, because we used a pretest/post-test design for a single group. This type of design permits inferring causal relations between the independent and dependent variables, though with some restrictions [70]. The small sample size ($n=8$) is another limitation because there is evidence that small reduced samples undermine internal and external validity, and so increase the likelihood of type I error, which decreases the power of the study. It is important to note that, however, that although the sample is small with only eight drug-naïve, mild-to-moderate AD patients, our findings do provide new and important data for understanding sleep disturbances and their associated treatments in cases of AD, since our subjects had not been treated previously with any neurological or psychiatric medication. Another limitation of our study is the lack of correction of multiple comparisons. Due to the small “ n ” we decided to illustrate all differences without such correction, though this could increase the level of speculation. Likewise, the use of measures of EEG correlations instead of coherence may be a methodological limitation, because coherence measures the co-variation between two signals as a function of frequency, taking into account both amplitude and phase changes between the signals involved, while correlation measures the co-variation between the signals as a function of time, considering only the phase relationship between the signals that are being analyzed, without considering amplitude.

We conclude that the short sleep onset related to melatonin intake in AD patients was associated with a lower RP of the alpha1 band and a higher RP of the delta band during the sleep onset period, mainly in the left hemisphere. These changes in EEG power were accompanied by a decreased degree of interhemispheric EEG coupling in the alpha1 band after melatonin administration. Our findings thus suggest that melatonin may have reduced sleep latency in these AD patients, probably due to an increase in the activity of GABAA receptors, mainly in the hypothalamus and basal forebrain. It is probable that structures like the suprachiasmatic nucleus, thalamic-cortical circuits and structures of the brain stem

related to sleep control and regulation—even in mild-to-moderate AD— are capable of reacting to the cascade of events that melatonin triggers on SOP.

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CONFLICT OF INTEREST

The authors have no conflict of interest to report.

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