Correlation between Topographic N400 Anomalies and Reduced Cerebral Blood Flow in the Anterior Temporal Lobes of Patients with Dementia

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Abstract. In Alzheimer’s disease (AD) patients, episodic memory impairments are apparent, yet semantic memory difficulties are also observed. While the episodic pathology has been thoroughly studied, the neurophysiological mechanisms of the semantic impairments remain obscure. Semantic dementia (SD) is characterized by isolated semantic memory deficits. The present study aimed to find an early marker of mild AD and SD by employing a semantic priming paradigm during electroencephalogram recordings. Event-related potentials (ERP) of early (P1, N1) and late (N400) word processing stages were obtained to measure semantic memory functions. Separately, baseline cerebral blood flow (CBF) was acquired with arterial spin labeling. Thus, the analysis focused on linear regressions of CBF with ERP topographical similarity indices in order to find the brain structures that showed altered baseline functionality associated with deviant ERPs. All participant groups showed semantic priming in their reaction times. Furthermore, decreased CBF in the temporal lobes was associated with abnormal N400 topography. No significant CBF clusters were found for the early ERPs. Taken together, the neurophysiological results suggested that the automatic spread of activation during semantic word processing was preserved in mild dementia, while controlled access to the words was impaired. These findings suggested that N400-topography alterations might be a potential marker for the detection of early dementia. Such a marker could be beneficial for differential diagnosis due to its low cost and non-invasive application as well as its relationship with semantic memory dysfunctions that are closely associated to the cortical deterioration in regions crucial for semantic word processing.

Keywords: Alzheimer’s disease, cerebral blood flow, event-related potential, magnetic resonance imaging, N400, semantic dementia, semantic memory, volumetry

INTRODUCTION

With the increasing population of elderly people, the prevalence of dementia increases from approximately 3% between 65 and 74 years to 25%–50% among those over 85 years [1, 2]. Alzheimer’s disease...
(AD), the most frequent type of dementia, is found in 70% of all patients affected [3]. Although the progressing deterioration of long-term memory, which affects episodic and semantic memory, is the major deficit in patients with AD, additional cognitive abilities are disturbed, such as language and executive functions [4, 5]. However, these latter abilities have been shown to also be degraded in other dementia types, such as frontotemporal dementia (FTD). FTD is characterized by a spectrum of non-Alzheimer’s dementias that mainly show frontal and/or temporal lobe degeneration [6]. The temporal variant of FTD has been described by a selective loss of semantic knowledge, and it is therefore referred to as semantic dementia (SD) [7, 8]. Alternatively, SD has been called the fluent variant of primary progressive aphasia [9].

Progress in neuroimaging techniques has recently allowed for the possibility of differential diagnosis of AD pathology by combining distinct biomarkers, such as the accumulation of amyloid-\(\beta\) (A\(\beta\)), increased cerebral spinal fluid (CSF) tau, and neuronal atrophy [10]. However, A\(\beta\) and tau markers can also be found in the elderly who do not develop the clinical syndrome of AD. In addition, the assessments of these biomarkers are costly and can be invasive for the patients (e.g., through the use of positron emission tomography (PET)). Furthermore, neuronal atrophy, which appears to occur only shortly before the clinical manifestation of AD, is rather difficult to distinguish from normal aging [10, 11]. For SD, diagnostic criteria that are based primarily on behavioral measures have been developed [9, 12]. In summary, it appears that the use of only imaging methods, such as PET and magnetic resonance imaging (MRI), is less suited for the preventive screening of the potential development of dementia in the symptom-free elderly on a routine basis. Consequently, there is still a need for cognitive measures that distinctively detect the probable emergence of the clinical syndromes of AD and SD [13–15]. For instance, Jack et al. [10] have stated that the number of studies that combine biomarkers is limited. Hence, the current study aimed at finding a biomarker for the clinical syndrome of dementia that is based on underlying pathology by investigating measures that reflect the cognitive symptomatology and the neuronal degeneration. However, because the combination of the clinical syndrome and the pathology is difficult to assess in the pre-symptomatic stage, we examined patients who were in an early symptomatic stage of AD or SD. This study must therefore be considered a first step in the development of a cost-efficient and non-invasive biomarker of dementia, as any candidate marker needs to be tested in a longitudinal study beginning at the pre-symptomatic stage.

In the following, a theoretical background of the cognitive measures that target the clinical syndrome, as well as the neurophysiological methods that assess neuropathology, is provided. Generally, language functions, communication, and everyday functioning rely strongly on an intact semantic memory. Even though semantic memory disturbances have been widely identified in patients with AD and can be measured with tasks, such as word fluency or object naming, the exact neurophysiological correlates of these disturbances remain unclear [16, 17]. Investigations of semantic memory dysfunctions with neurophysiological measures are thus needed to identify markers that can be used for the early clinical diagnosis of patients with AD. In particular, semantic memory functions are often examined through priming paradigms that are established research instruments that are utilized for the assessment of rather automatic semantic memory functions with minimized influence of explicit cognitive processes [18]. This is advantageous in order to avoid confounding factors, such as working memory or more general executive processes, especially because they co-occur as deficits in the dementia types. In particular, semantic priming is characterized as the facilitated retrieval of (target) words which are preceded by contextually related words, so-called primes. This effect is commonly detected by shorter reaction times (RTs) to related (e.g., forest - tree) than to unrelated (e.g., frog - guitar) word pairs. The resulting semantic priming effect has been attributed to the spread of neural activation within the semantic memory network [19].

Previous behavioral priming studies that have been conducted on patients with AD and SD have reported diverging results, including reduced [20], normal [21, 22], and increased priming [23], compared to healthy participants. Despite these inconsistencies, semantic priming can be regarded as a valuable tool for investigating the integrity of semantic memory functions if the paradigm is carefully designed and influencing factors (e.g., stimulus timing, word versus sentence task) are taken into account [24].

In addition to the behavioral domain, semantic priming effects have been examined by means of electrophysiological markers, such as event-related potentials (ERPs). Wirth et al. [25] have demonstrated an automatic semantic priming effect in healthy participants that occurs between 120–190 ms after target-word onset (early ERP). During this period, the ERP components labeled as P1 and N1 can be observed, and these are possibly functionally linked
with the automatic spread of activation in the semantic system. Furthermore, in numerous studies, the well-established controlled semantic priming effect has been found approximately between 250-500 ms (late ERP). This time frame coincides with the ERP component referred to as N400, thus reflecting a semantic integration stage [26, 27].

While investigating semantic processing in patients with AD, the majority of studies have found reduced N400 amplitudes with delayed latencies compared to those in elderly controls (EC) [28]. Similarly, Schwartz et al. [29] have shown comparable N400 component amplitudes but smaller priming effects in patients with AD compared to those in young and elderly controls. Furthermore, their data for mixed auditory and visual stimuli with a rather long stimulus-onset asynchrony of approximately 1,000 ms have indicated that the priming effect occurred later in the patients with AD than in the healthy groups. However, they concluded that, despite the alterations in patients with AD, their semantic network does not seem to be broken down severely, as shown by a normal N400 component amplitude. Similarly, Iragui and colleagues [30] have shown reduced and delayed N400 priming in patients with AD with a context-phrase task. According to those authors, the difference might have occurred due to altered attentional processes or weaker associative links that were related to more advanced age.

Ford et al. [31] have found, while also assessing sentence processing in patients with AD, reduced N400 priming effects in the semantic but not in the phonemic task and delayed latencies in both conditions. Although these results appeared to demonstrate a distinct semantic memory alteration in patients with AD, the fact that their semantic condition involved a delayed-recognition test might raise doubts of whether their results were confounded by episodic memory processes. Similarly, Hurley and colleagues [32] have shown that altered N400 amplitudes are evoked by picture-picture and picture-word matching tasks in patients with the semantic variant of primary progressive aphasia compared to controls. The only study that has investigated the early ERP components (N1, P2) of semantic processing besides the late N400 in patients with AD so far has been the study conducted by Revonsuo and colleagues [33]. They found a comparable congruity effect between patients with AD and controls in P2. In contrast, this effect was smaller in the N400 in the AD group compared to the control group. Therefore, these authors have claimed that early lexical processes are preserved in patients with AD, whereas semantic-conceptual stages are impaired. In accordance, Ford et al. [34] have found differing topographic N400 congruity effects in patients with AD compared to controls. Nevertheless, they demonstrated that the N400 priming effect and scalp distribution were stable across patients with AD, regardless of whether they were able to name a picture correctly or not. This latter result has been replicated by Auchterlonie et al. [35]. Thus, these results have provided evidence that patients with AD have an impaired access to semantic concepts, although the knowledge remains intact. Moreover, Olson et al. [36, 37] have shown that an abnormal N400 is associated with an increased risk for conversion from mild cognitive impairment to AD within three years.

In contrast to the studies that have shown altered ERPs in patients with AD, there have been findings of equivalent N400 measures in patients with AD. For example, Hamberger et al. [38] who also employed a sentence task found that the N400 was modulated to the same degree by semantic relation in probable AD patients and young controls. They assumed that the semantic deficits in patients with AD were expressed even at a later processing stage than the N400. Despite the considerable number of studies that have investigated semantic ERPs in patients with AD, data on the early ERPs (i.e., P1/N1) of semantic priming that are induced by visual stimuli in patients with AD and SD are missing.

Although electrophysiological data represent a direct measure of brain activity, it is hard to draw conclusions from this data of the underlying structural changes and, thus, the pathology of AD and SD in comparison to controls. Commonly, brain atrophy in patients with AD and SD has been measured with structural MRI with voxel-based morphometry (VBM) [39–44].

Even though the well-circumscribed grey matter (GM) volume losses in these patients appear to have an important relationship with the patients’ cognitive deficits, volumetric measures alone are not the optimal way to detect degenerative diseases in the pre-clinical phase, as stated above. In particular, comparisons of different biomarkers have been advised in order to validate their application [10]. One possibility could be an investigation of the functional integrity of the brains of early or pre-dementia patients with cerebral blood flow (CBF) measurements [45, 46]. More recently, MRI-based arterial spin labeling (ASL) has allowed assessments of the resting-state CBF in a non-invasive fashion in healthy participants and patients [14, 47]. In accordance with this advantage, the current study employed ASL in addition to a standard VBM analysis.
The most prominent findings of the previous studies of patients with AD were reduced CBF in the inferior parietal lobe, the posterior cingulate gyrus, and the middle frontal gyrus, as well as the inferior temporal cortex, compared to controls [48, 49]. These results are in line with those of studies that have used the more classical, but invasive, PET method (e.g., [47]). However, hypermetabolism has been reported in the hippocampus and other medial temporal structures, as well as in the anterior cingulate gyrus [49–51]. Hypermetabolism that coincides with GM atrophy has been suggested to reflect compensatory neural activity, inflammation or the increased production of vasodilators [49]. No ASL studies have been conducted on patients with SD, but, a fluorescent glucose PET study that was conducted by Diehl et al. [52] has revealed reduced glucose metabolism in the entire left temporal lobe and the right temporal pole in patients with SD.

Overall, despite the asynchronous onsets of the different biomarkers of dementia, the clinical syndrome of AD and SD appears to be strongly related to its pathology, as shown by the structural and functional aberrations that involve language-related areas among others in these patients.

In the present study, the above-circumscribed neurophysiological methods (i.e., ERP, VBM, and ASL) were applied in order to differentiate semantic memory dysfunctions in patients with AD and those with SD and relate them to the underlying resting CBF. In particular, this is the first study that has directly related ERPs of semantic processing to the individual CBF findings in early dementia patients. Hence, it aimed to identify a measure of deviant semantic word processing that reflects the symptomatology of the clinical syndromes of AD and SD and that is associated with brain regions showing altered blood flow.

The following hypotheses were made for the present study. First, in order to verify that the semantic paradigm conducted in this study actuated semantic processing, a robust semantic priming effect of RT was expected, at least for EC subjects and patients with AD. Second, the replication of the distinction of early and late ERPs in the semantic word processing of ECs was anticipated. Third, both GM volumes and regional CBF were hypothesized to be comparable to those found in previously published studies. In patients with AD, medial temporal, parietal, and basal GM atrophies were expected, while, in patients with SD, the volume of the temporal pole and the adjacent lateral temporal gyri, in particular, were predicted to be decreased. Moreover, in patients with AD, reduced CBF was expected in the parietal lobe, posterior cingulate gyrus, middle frontal gyrus, and inferior temporal cortex. In contrast, hypermetabolism was expected in the medial temporal areas. As outlined above for patients with SD, hypometabolism was anticipated to converge with findings of GM atrophy, particularly in the anterior temporal lobe. Fourth, the following brain areas were expected to be involved in the combination of ERP and CBF: for the early ERPs, the occipital and posterior temporal lobes, and, for the late ERPs, the anterior temporal lobes [25, 53–55]. Due to the lack of previous studies on early ERPs in patients with AD and SD in general, it was hard to predict the outcome of the ERP analysis. Nevertheless, an altered N400 was expected in patients with AD, as described above, and, if the patients with SD had a loss of semantic knowledge [40], all analyzed ERPs were predicted to be changed because both the spread of activation and word retrieval would have been disturbed.

MATERIALS AND METHODS

Participants

A total of 48 participants were examined (22 EC, 19 AD, 7 SD). However, due to an inability to perform the task (4 ADs), not fulfilling the diagnostic criteria (1 AD, 2 SDs), excessive MRI artifacts (1 EC), technical problems (1 AD), or an incidental finding of a tumor (1 EC), 10 participants had to be excluded from the data analysis, thus resulting in a sample of 38 participants (19 EC, 14 AD, 5 SD). The reason for the small SD group was that recruitment was complicated due to its relatively rare prevalence, its difficult diagnosis, and the absence of cognitive abilities in the patients to understand the study procedure. All were native speakers of Swedish, and their vision was either normal or corrected to normal. The study complied with the Declaration of Helsinki and was approved by the Regional Ethics Committee of Stockholm, Sweden, and all participants provided written informed consents.

The participant recruitment was different for each group. While the ECs were recruited by advertisement, patients with AD were contacted while they were in treatment at the Memory Clinic of the Geriatric Department at Karolinska University Hospital in Huddinge, Sweden. Their diagnoses were made by expert clinicians and were in accordance with the ICD-10 criteria [56]. Patients with SD were recruited from all over Sweden in accordance with the criteria by Neary et al. [12]. As part of the standard clinical procedure, the patients underwent physical and psychiatric medical examinations, including standard blood analyses.
structural neuroimaging examinations, lumbar puncture, as well as a neuropsychological assessment. Apart from the patients’ AD or SD diagnosis, as well as concurrent medication, none of the participants was affected by any neurological or psychiatric disease or taking medication affecting the central nervous system. Furthermore, a resting electroencephalogram (EEG) was measured in order to rule out abnormal EEG patterns, such as signs of spikes and waves.

Stimulus material and task

The semantic priming paradigm employed in this study was adopted from Grieder and colleagues [24]. It involved a lexical decision (LD) task and was composed of stimulus pairs containing nouns and non-words. The stimulus material varied by two experimental factors (relatedness and concreteness) with two levels (i.e., unrelated [U], related [R], concrete [C], or abstract [A]; Fig. 1B). This resulted in four experimental conditions of interest: UC, UA, RC, and RA. For the exact task construction and validation of the stimuli, please refer to Grieder et al. [24]. Generally, the paradigm consisted of 160 word (noun) pairs (40 per condition), 160 matched pronounceable non-word–noun and noun–non-word pairs and 32 filler word pairs (352 stimulus pairs altogether). The total number of stimulus pairs differed slightly from that in Grieder et al. [24] in order to keep the task duration as short as possible (approximately 21 min), while the stimulus-onset asynchrony was prolonged (700 ms, Fig. 1A). In detail, stimulus pairs appeared on a computer screen in sequential order (white Arial bold font, size 28, on black background). At a distance of 90 cm from the screen, the visual angle of the stimuli ranged from 0.382° to 0.637° in height and 0.446° to 4.263° in width. After a red fixation cross appeared (400 ms), the prime or non-word appeared for 650 ms. Next, an inter-stimulus interval of 50 ms was followed by the target or non-word, which was displayed until the participant responded or 1,500 ms at maximum. Succeeding the target, a white fixation cross appeared for another 1,500 ms to complete one stimulus trial. The participants were instructed to press one of two buttons on a button box immediately after the target appeared to indicate whether the stimulus pair contained a non-word at either the prime or target position. In particular, in cases in which the stimulus pair contained two words, the participants had to press the rightmost button with the index finger of their dominant (right) hand, whereas if a non-word appeared at either the prime or target position, a button press on the leftmost button was required with the index finger of the non-dominant (left) hand. The RT was determined as the elapsed time in ms between the target stimulus onset and the participant’s button press. The task was presented with E-Prime software (version 1.2, Psychology Software Tools, Inc., Pittsburgh, PA, USA) which logged the RT online.

Procedure

The examinations of the participants were divided into two separate sessions; one involved the neuropsychological testing and the EEG, and the other involved the MRI measurement. The first session, which was
conducted at the phonetic laboratory of the Department of Linguistics at Stockholm University, started with an assessment of the participants’ medical history. The subsequent neuropsychological examination included a vision screening, the Mini-Mental State Examination (MMSE), Boston Naming Test (BNT), Animal Fluency test (AF), Clock Task (CT, read and construct), and a computerized visuo-motor RT task. Additionally, patients with AD and those with SD were tested with the Global Deterioration Scale (GDS) and the Cornell Depression Scale (CDS).

After the neuropsychological examination, the participants were seated on a chair in an electrically shielded room. As a next step, a resting EEG was measured for 6 min and 40 s with three periods of eyes closed (2 min each) and two periods of eyes opened (20 s each). Then, the LD task was introduced by means of a practice run. In particular, the participants read the task instructions on the screen and made LDs on 30 stimulus pairs (15 noun-noun and 15 noun–non-word pairs). The subsequent experimental LD task with simultaneous EEG/ERP recordings was only initiated if the participants were successful in the practice run.

The second session was performed at the Karolinska University Hospital in Huddinge, Sweden, where the MRI recordings were conducted. The participants were instructed to lie motionless in the scanner without falling asleep. In order to minimize motion artifacts, the participants’ heads were carefully fixed by means of foam cushions. At first, a structural T1-weighted sequence was run. Second, a pseudo-continuous ASL (pCASL) measurement was conducted which concluded the data acquisition.

Behavioral data analysis

Possible group differences in demographics and neuropsychological tests were analyzed with non-parametric Kruskal-Wallis tests. Only the four word conditions, UC, UA, RC, and RA, were used for the analysis, and the filler and non-word conditions were not included. Offline, the median RT was calculated for each word condition and participant. Subsequently, a repeated-measures analysis of variance (ANOVA) with a $2 \times 2 \times 3$ factorial design (relatedness and concreteness as within-subject factors; group as between-subject factor) was conducted. Potential interactions were further disentangled by the Scheffé post-hoc test. The $\delta$-prime was calculated as a measure of individual task performance [57]. The resulting $z$-transformed scores were then subjected to a one-way ANOVA with a subsequent Scheffé post-hoc test.

EEG/ERP recording and preprocessing

Electrophysiological measurements were conducted with a high-impedance 128-channel HydroCel Geodesic Sensor Net connected to a Net Amps 300 amplifier (Electrical Geodesics, Inc., Eugene, OR, USA). A potassium-chloride solution was applied to the electrodes in order to keep the impedances below 50 kΩ, and they were checked before the resting EEG and the ERP-EEG recordings. The recording reference was Cz, and the ground electrode was positioned between CPz and Pz. A fixed sampling rate of 20,000 Hz was low-pass filtered at 4,000 Hz and further down sampled online to 250 Hz. Preprocessing was done with Vision Analyzer (Version 1.05, Brain Products GmbH, Gilching, Germany). An Independent Component Analysis [58] was computed to correct for eye movements and remove artifacts that were caused by eye blinks, repeatedly occurring electrode shifts, and/or cardio-ballistics. Channels containing muscle or other irregular artifacts were interpolated (order of splines = 4; maximal degree of Legendre Polynomials = 10; Lambda = 0.00001). Before the average reference was computed, the four channels located under each eye and ear were excluded from further analysis. The remaining epochs containing artifacts were removed by manual inspection. Moreover, an offline band-pass filter was applied at 0.5–18 Hz (24 dB/oct).

With the aim of extracting ERPs from the EEG, all experimental stimuli plus participant responses were marked online. Hence, segments starting from target-word onset and ending 1,000 ms after target-word onset were derived offline. Segments corresponding to false responses were rejected. Following this, the individual ERPs for the experimental conditions (UC, UA, RC, and RA) were averaged. Additionally, the individual average epoch over all conditions was derived, and, finally, the equivalent Global Field Power (GFP) [59] was calculated.

ERP analysis

The ERP analysis performed in this study mainly involved the two steps described in detail below. The aim was to obtain a suitable ERP measure that can be correlated with CBF. Therefore, the rationale was to find an appropriate measure reflecting the extent of deviation in semantic word processing in the healthy
group ERPs. For this reason, a topographic approach appeared plausible because it accounted for the signals from all electrodes and identified neural activation modulations of the underlying source distribution [60]. As a consequence, the individual ERP topographies were spatially correlated with the mean ERP topography of the EC group as a measure of topographical similarity or deviation, respectively.

However, because the early ERP components (especially P1) are known to reflect visual perceptive processes, it was essential to verify that the P1 and N1 (as well as the N400) of the current study involved semantic processes by means of semantic priming, as demonstrated in Wirth et al. [25]. Therefore, a topographic ANOVA (TANOVA) that compared the individual averaged epochs of the unrelated and related word-pair conditions of the EC was conducted. The TANOVA is a non-parametric randomization test of reference-independent topographic differences [60]. In particular, 5,000 randomization runs were computed with a $p$-threshold of 0.05 (for details, see [24, 61, 62]).

**Peak detection**

For each ERP of interest (P1, N1 and N400), an automated peak detection that searched for local maxima was conducted with the Brain Vision Analyzer software. For this purpose, a pre-defined time window for each ERP was needed in order to avoid an overlap and subsequent confusion of the peaks to be detected. To this end, a separate topographic cluster analysis (microstates) [63] involving a $k$-means algorithm was performed on the mean epoch of the healthy participants with the Ragu software [61]. The resulting onsets and offsets of the microstates (corresponding to the P1, N1, and N400) were assigned as a time-frame limiter to the peak detection. In particular, the peaks were determined on the GFP and applied to all channels in order to extract the three peak topographies of each participant. Furthermore, the peak topographies were normalized (GFP = 1) in order to remove electrical field strength differences from the topographies. Finally, all extracted topographies of the ECs were averaged in order to create the ERP topography template.

**Topographic component recognition**

Topographic component recognition (TCR) [64] was employed in order to obtain a parameter of the individual topographic similarities (i.e., spatial correlation) of the ERPs to the topography templates of the ECs. The individual ERP topographies that were derived from the peak detections were simply correlated with the group topography of the ECs (i.e., template map) with a self-written MATLAB script. The outcome variable of the TCR was one $r$ value per ERP and participant.

The advantage of the TCR compared to conventional single-channels or channel-groups analyses shall be briefly outlined. The TCR analysis extracts the strength of a component as a weighted mean of all electrodes, whereas the weights are given by the template map. An analysis of single channels or group channels is a very similar procedure, with the only difference being that the weights of the included electrodes are set to 1, and the weights of the excluded electrodes are 0. Single-channel and group-channel analyses are thus special cases of topographic analyses, with predefined binary template maps. If a template map that covers the whole scalp is given, as was the case in this study, a reduction to the binary form would possibly reduce the statistical power of the analyses. In other words, if only a few electrodes accounted for the effect of interest, the template map would give all the weights to those electrodes, which is very similar to the use of just those few electrodes.

**MRI recording**

A 3T Siemens Magnetom Trio MR Scanner (Siemens AG, Erlangen, Germany) was used for MRI data acquisition. The parameters of the T1-weighted magnetization-prepared rapid acquisition gradient-echo (MPRAGE) sequence were set as follows: repetition time (TR)/echo time (TE), 1,900 ms/2.57 ms; 176 sagittal slices; slice thickness, 1.0 mm; field of view (FOV), 230 $\times$ 230 mm; matrix size, 256 $\times$ 256; leading to a voxel dimension of 0.9 $\times$ 0.9 $\times$ 1.0 mm. The $p$CASL measurement was applied [65, 66] with these parameters: TR/TE/post-label delay ($\omega$)/tagging duration ($\tau$) [ms], 3500/18/1170/1600, 18 horizontal slices; FOV, 230 $\times$ 230; matrix size, 64 $\times$ 64 and voxel size, 3.6 $\times$ 3.6 $\times$ 6.0 mm; gap between slices, 0.9 mm; slice acquisition time, 45 ms and TA, 8 min 22 s.

**VBM**

Processing of the structural images from the MPRAGE sequences was performed with statistical parametric mapping software (SPM8, Wellcome Laboratory of Imaging Neuroscience, London, England; http://www.fil.ion.ucl.ac.uk) in order to test for regional differences in GM volume between the
Thus, for the VBM analysis, the optimized protocol described in Good et al. [68] was applied.

Thus, the following computation steps were conducted. First, the structural images were automatically segmented into GM, white matter (WM) and CSF. Next, spatial normalization was applied [leading to Montreal Neurological Institute (MNI) normalized images], which was followed by the modulation option that was chosen for this study in order to preserve the volume of each tissue within a voxel [68]. Finally, the segmented, normalized, and modulated images were smoothed with an isotropic Gaussian kernel of 10 mm Full Width at Half Maximum (FWHM). Additionally, the total intracranial volume (TIV) was derived from the addition of the GM, WM, and CSF volumes of each participant, and it was used as a covariate in the statistical VBM analysis.

**CBF quantification**

The pCASL images were preprocessed by realignment correction for motion artifacts, coregistration to the individual structural images, and normalization into MNI space. While the preprocessing steps were done with SPM8 routines, the quantification was computed with in-house MATLAB scripts (Version 7.6; The MathWorks Inc., Natick, MA, USA). The individual regional CBF values were computed with the following quantification equation:

\[
\text{CBF} = \frac{\lambda \Delta M}{\alpha M_0 \tau_{lb}} \cdot \left(1 - e^{-\frac{w}{T_{1lb}}} - e^{-\frac{\tau + w}{T_{1lb}}}ight)
\]

According to Wu et al. [65], the blood/tissue water partition coefficient (\(\lambda\)) was fixed at 0.9 (g/ml), the tagging efficiency (\(\alpha\)) at 0.95 and the decay time for labeled blood (\(T_{lb}\)) for 3.0 T magnetic fields at 1,490 ms. \(M_0\) was the equilibrium brain tissue magnetization images [69, 70]. \(\Delta M\) was obtained by simply subtracting the label from the control images. The derived difference was proportional to the CBF [71].

**Voxel-based statistics**

For the VBM analysis, modulated GM images were employed in a voxel-by-voxel fashion for group comparisons with an analysis of covariance (ANCOVA), with TIV as the covariate. The statistical approach was similar to that of Focke et al. [73] with a threshold of \(p < 0.0001\) (uncorrected) applied to the \(F\)-statistics. The resulting clusters were corrected for multiple comparisons with a family-wise error rate (FWE) of \(p < 0.05\). Post-hoc \(t\)-tests were conducted in order to inspect the GM volume differences (Bonferroni corrected \(p\)-threshold) between AD versus EC, SD versus EC and AD versus SD.

For the voxel-based analysis of CBF, individual GM masks were created in order to conduct the CBF statistics that were based on GM-corresponding voxels only. The resulting masked CBF images were subjected to an ANCOVA with the global GM CBF as a covariate. Equivalent to the VBM analysis, \(F\) and \(t\) statistics were evaluated in order to obtain significant group differences in CBF.

Finally, for each ERP of interest (P1/N1/N400), a voxel-based linear regression was employed with GM-masked CBF images and individual \(r\) values of the TCR as the regressor [74]. Global CBF was included as a covariate.

**Correlations of the physiological parameters with the behavioral variables**

In order to investigate the relationship of the neuropsychological test scores with the CBF and ERP variables, a Spearman rank correlation was conducted.

**Results**

**Behavioral data**

The demographics, neuropsychological scores, and statistics are listed in Table 1. Neither age nor education was significantly different between the groups. Therefore, these variables were not used as covariates. Second, the neuropsychological tests demonstrated the following selective deficits in the patient groups: while the MMSE, BNT, AF, and VF scores were reduced in patients with AD and those with SD, they performed as well as the EC in the CT tasks. Note that the group-wise post-hoc Mann-Whitney tests showed significant differences in the MMSE, BNT, AF, and VF scores between EC and AD, EC and SD as well as AD and SD at \(p < 0.01\), except for the MMSE and VF scores.
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Table 1

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<td>AF</td>
<td>23.8</td>
<td>6.3</td>
<td>14.9</td>
<td>2.2</td>
<td>9.0</td>
<td>6.6</td>
</tr>
<tr>
<td>VF</td>
<td>21.6</td>
<td>5.8</td>
<td>12.4</td>
<td>4.3</td>
<td>9.4</td>
<td>7.4</td>
</tr>
<tr>
<td>CT construct</td>
<td>3.8</td>
<td>1.4</td>
<td>3.6</td>
<td>0.8</td>
<td>3.3</td>
<td>2.0</td>
</tr>
<tr>
<td>CT read</td>
<td>4.6</td>
<td>0.9</td>
<td>4.3</td>
<td>1.2</td>
<td>4.8</td>
<td>0.4</td>
</tr>
</tbody>
</table>

EC, elderly controls; AD, Alzheimer’s disease; SD, semantic dementia; SD, standard deviation; MMSE, Mini-Mental State Examination; BNT, Boston Naming Test; AF, animal fluency; VF, verb fluency; CT, clock task.

which did not differ significantly between the AD and SD groups.

Figure 2 depicts the descriptive group RTs per word condition, and Table 2 shows the ANOVA results. Generally, all groups showed semantic priming (i.e., relatedness effect, shorter RT for related words compared to RTs for unrelated words). Consequently, these results indicated that the participants processed the stimulus material semantically and not only lexically, as intended. This finding is important for the correlations of the task-related ERPs and the CBF in brain structures that are associated with semantic processing. Note that the concreteness effect was not of interest in this study. More importantly, a group main effect together with the post-hoc test showed that the SD group exhibited longer RTs than the EC and AD groups. For accuracy, the one-way ANOVA revealed a significant group effect of d-prime scores (Table 2). The Scheffé post-hoc test confirmed that all groups differed significantly from each other in task performance, with the EC group performing best and the SD group performing worst (EC-AD = 0.87, SE = 0.22, p < 0.01; EC-SD = 1.90, SE = 0.32, p < 0.001; AD-SD = 1.03, SE = 0.33, p < 0.05).

**ERP**

Figure 3 depicts a first approach to the ERP data analysis that shows example electrode waveforms (F3, T6, and Pz) between the unrelated and related word conditions for each participant group. Additionally, the GFP waveform illustrates the electrical field strength of all electrodes over time. What can be drawn from these waveforms as well as from the topographic map series (Fig. 4A) is that the early P1 and N1 components occurred in all three groups, although the amplitudes might have been reduced in patients with SD (see for example electrode T6 in Fig. 3). Moreover, amplitude differences can be observed between the unrelated and related word condition in the P1 and N1 components, especially pronounced in the N1. Also, the waveforms indicate that the amplitude modulation between unrelated and related word pairs in the time window of the N400 component was strongest in the healthy controls.
Table 2
Statistical analyses of reaction time, accuracy, and topographic component recognition

<table>
<thead>
<tr>
<th>Reaction times</th>
<th>ANOVA</th>
<th>F</th>
<th>df</th>
<th>p</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Relatedness</td>
<td>35.936</td>
<td>1</td>
<td>&lt;0.001 ***</td>
<td></td>
</tr>
<tr>
<td>Concreteness</td>
<td>5.961</td>
<td>1</td>
<td>&lt;0.05 *</td>
<td></td>
</tr>
<tr>
<td>Relatedness × group</td>
<td>1.805</td>
<td>2</td>
<td>0.18</td>
<td></td>
</tr>
<tr>
<td>Concreteness × group</td>
<td>0.173</td>
<td>2</td>
<td>0.84</td>
<td></td>
</tr>
<tr>
<td>Relatedness × concreteness</td>
<td>3.480</td>
<td>1</td>
<td>0.07</td>
<td></td>
</tr>
<tr>
<td>Relatedness × Concreteness × group</td>
<td>1.003</td>
<td>2</td>
<td>0.38</td>
<td></td>
</tr>
<tr>
<td>Group</td>
<td>18.180</td>
<td>2</td>
<td>&lt;0.001 ***</td>
<td></td>
</tr>
</tbody>
</table>

Post-Hoc Test (Scheffé)

<table>
<thead>
<tr>
<th>Mean difference</th>
<th>SE</th>
<th>p</th>
</tr>
</thead>
<tbody>
<tr>
<td>EC – AD</td>
<td>–51.9</td>
<td>15.1</td>
</tr>
<tr>
<td>EC – SD</td>
<td>–303.4</td>
<td>50.4</td>
</tr>
<tr>
<td>AD – SD</td>
<td>–251.5</td>
<td>52.3</td>
</tr>
</tbody>
</table>

Accuracy

<table>
<thead>
<tr>
<th>Hit rate</th>
<th>False alarm rate</th>
<th>d’ value</th>
</tr>
</thead>
<tbody>
<tr>
<td>0.98</td>
<td>0.05</td>
<td>3.98</td>
</tr>
<tr>
<td>0.03</td>
<td>0.06</td>
<td>3.11</td>
</tr>
<tr>
<td>0.06</td>
<td>0.11</td>
<td>0.47</td>
</tr>
<tr>
<td>0.03</td>
<td>0.05</td>
<td>0.38</td>
</tr>
<tr>
<td>0.06</td>
<td>0.29</td>
<td>0.29</td>
</tr>
<tr>
<td>3.738</td>
<td>17.495</td>
<td>20.239</td>
</tr>
<tr>
<td>2</td>
<td>2</td>
<td>2</td>
</tr>
</tbody>
</table>

Topographic component recognition

<table>
<thead>
<tr>
<th>P1</th>
<th>N1</th>
<th>N400</th>
</tr>
</thead>
<tbody>
<tr>
<td>Mean</td>
<td>SD</td>
<td>Mean</td>
</tr>
<tr>
<td>0.76</td>
<td>0.19</td>
<td>0.66</td>
</tr>
<tr>
<td>0.62</td>
<td>0.29</td>
<td>0.41</td>
</tr>
<tr>
<td>0.61</td>
<td>0.27</td>
<td>0.25</td>
</tr>
</tbody>
</table>

EC, elderly controls; AD, Alzheimer’s disease; SD, semantic dementia; SD, standard deviation.

and attenuated in patients with AD. For patients with SD, the N400 can be hardly identified in the waveforms or the topographic maps. The GFP of the AD group appeared to be comparable with that of the healthy controls in the P1 time window, but seemed to be decreased in the later ERP components. For patients with SD, the GFP seems to be reduced especially in the unrelated word pair condition during the P1 and N1 components, while the image is more diffuse in later time windows.

In the statistical ERP analysis, Fig. 4B illustrates that the TANOVA detected the early semantic priming effect that was measured by the topographical differences between 94 ms and 302 ms after target onset. Furthermore, there was a late topographical semantic priming effect between 382 ms and 546 ms. Thus, all ERPs of interest (P1, N1, and N400) reflected semantic processing, as demonstrated by the overlap of the significant TANOVA epochs with the ERPs marked in Fig. 4C. In detail, Fig. 4C displays the temporal assignment of the eight microstates that were provided by the k-means cluster analysis overlaid with the GFP of the mean epoch of the EC group. Furthermore, the P1, N1, and N400 were labeled, as well as their corresponding time frame of occurrence (i.e., onset and offset). Note that, for the P1, the first GFP trough at 56 ms was chosen as the onset, instead of the 0 ms resulting from the clustering algorithm, which did not appear to be appropriate for the P1. This view was supported by the fact that the early TANOVA effect did not start before 94 ms and that no studies have reported semantic processing before 50 ms after stimulus onset [25, 53, 75]. Additionally, the group maps (templates for the EC group) of the P1, N1, and N400 of each group are depicted as topographical maps in Fig. 4D. Furthermore, as can be derived from Table 2, the Kruskal-Wallis test of the TCR resulted in significantly different correlations between the groups in the N400 only. The subsequent Scheffé post-hoc test showed that this effect was caused by differences between the EC and AD groups as well as between the EC and SD groups (EC-AD = 0.36, SE = 0.10, p < 0.01; EC-SD = 0.62, SE = 0.15, p < 0.01; AD-SD = 0.26, SE = 0.15, p = 0.25).

VBM

The participant groups did not differ in total GM volume as shown by the Kruskal-Wallis test (µ² (2, 38) = 2.05, p = 0.36). However, the voxel-based statistics resulted in five significant clusters of differing
GM volumes (Table 3). As shown in Fig. 5A visualized with xJView toolbox, http://www.alivelearn.net/xjview, the largest cluster (F peak at X = −30, Y = −6, Z = −34; MNI) extended from the left fusiform gyrus over the parahippocampal, hippocampal, and inferior temporal gyri and the temporal pole to the insula. Furthermore, even the left putamen and amygdala were involved. Additionally, in order to investigate the possible regional GM volume differences between the groups within this cluster, a voxel-wise T-test was conducted. As expected, between the EC and AD groups, the GM volume differed in the hippocampus, parahippocampal area, amygdala, and inferior temporal lobe (Fig. 5B). Furthermore, patients with SD showed reduced GM volume in the entire cluster compared to the other two groups. In the whole-brain VBM analysis, a comparable cluster can be observed in the right hemisphere, but to a smaller voxel extent (F peak at X = 42, Y = 14, Z = −30). In addition, the SD group exhibited enhanced GM volume in the left inferior parietal lobe compared to the AD group. Next, the SD group exhibited increased GM volume in the right middle occipital gyrus compared to the other groups. Finally, the AD group had a lower GM volume in the right middle frontal gyrus compared to the EC group.

CBF

The AD group had lower global GM CBF compared to the EC group, as revealed by the Scheffé post-hoc test (EC-AD = 11.19, SE = 2.34, p < 0.001*** that was preceded by the Kruskal-Wallis test [χ² (2, 38) = 13.65, p < 0.01**]. As in the VBM analysis, the largest cluster that was found with the CBF statistics extended further than the F peak (X = −54, Y = 6, Z = −32) only would indicate (Table 4). Instead, this cluster ranged from the left temporal pole over the fusiform gyrus to the hippocampus and the parahippocampal region (Fig. 5C). For this cluster, the t-tests demonstrated significantly decreased CBF in the AD and SD groups compared to the EC group. Similarly, reduced CBF was also observed in the left inferior temporal gyrus in both patient groups. Moreover, they exhibited
Fig. 4. A) Descriptive topographic grand average maps of unrelated and related word conditions for each participant group are depicted. B) Topographical relatedness (priming) effect of the topographic analysis of variance (TANOVA) in the elderly control (EC) group. The grey areas indicate non-significant topographic differences. The white areas show time epochs of the topographic differences without fulfilling the statistical criterion of minimal duration (i.e., were shorter than 0.95 of all resulting effect durations). Hence, the white areas could have occurred by chance only. The green areas reflect significantly differing topographies between unrelated and related word pairs. C) Microstate cluster analysis results in the 1,000-ms epoch after target-word onset overlaid with the mean Global Field Power (GFP) of the EC group. D) The group event-related potentials depicted as a topographical map. The maps of the EC group served exclusively as templates for the topographic component recognition. Remark: The low amplitudes are due to GFP normalization. AD: Alzheimer’s disease. SD: semantic dementia.

Table 3
Voxel-based-morphometry analysis of the anatomical regions that correspond to the Montreal Neurological Institute (MNI)-coordinates at the F peak, the number of involved voxels and the peak F- and pFWE-corr values. Therefore, other brain structures were involved in the clusters, especially in the large ones (see text). Additionally, the post-hoc T-test results are listed with T and p values.

<table>
<thead>
<tr>
<th>Anatomical region</th>
<th>X</th>
<th>Y</th>
<th>Z</th>
<th># of voxels</th>
<th>F (pFWE-corr)</th>
<th>EC-AD T (p)</th>
<th>EC-SD T (p)</th>
<th>AD-SD T (p)</th>
</tr>
</thead>
<tbody>
<tr>
<td>L fusiform gyrus</td>
<td>−30</td>
<td>−6</td>
<td>−34</td>
<td>7180</td>
<td>63.24 (&lt;0.001***)</td>
<td>2.56 (0.016)</td>
<td>7.58 (&lt;0.001***)</td>
<td>5.87 (&lt;0.001***)</td>
</tr>
<tr>
<td>R middle temporal pole</td>
<td>62</td>
<td>14</td>
<td>−30</td>
<td>4692</td>
<td>30.59 (&lt;0.01**)</td>
<td>2.78 (0.013)</td>
<td>5.59 (&lt;0.001***)</td>
<td>3.77 (&lt;0.01*)</td>
</tr>
<tr>
<td>R middle occipital gyrus</td>
<td>18</td>
<td>−94</td>
<td>12</td>
<td>98</td>
<td>28.18 (&lt;0.01*)</td>
<td>0.23 (0.82)</td>
<td>4.15 (&lt;0.01*)</td>
<td>4.04 (&lt;0.01*)</td>
</tr>
<tr>
<td>L inferior parietal lobe</td>
<td>−44</td>
<td>−56</td>
<td>42</td>
<td>143</td>
<td>26.12 (&lt;0.01*)</td>
<td>2.65 (0.013)</td>
<td>−2.44 (0.04)</td>
<td>−4.49 (&lt;0.01*)</td>
</tr>
<tr>
<td>R middle frontal gyrus</td>
<td>32</td>
<td>36</td>
<td>30</td>
<td>95</td>
<td>24.18 (&lt;0.01*)</td>
<td>4.46 (&lt;0.001***)</td>
<td>−0.71 (0.5)</td>
<td>−2.32 (0.07)</td>
</tr>
</tbody>
</table>

T-test crit. p-value: p < 0.01; L, left; R, right.
decreased CBF in the left insula, while only the SD group’s CBF was lower in the left putamen and only the AD group’s CBF was lower in the left globus pallidus. On the contralateral side, considerably smaller clusters that involved only the right middle temporal pole and the inferior temporal gyrus were found. In the former cluster, only the SD group differed from the EC group, while, in the latter cluster, both the AD and SD groups exhibited decreased CBF.

Linear regression CBF-ERP

First, the linear regression of P1 and N1 yielded no significant clusters. Therefore, only results referring
Table 4
Cerebral blood flow analysis of the anatomical regions that correspond to the MNI coordinates at the Tpeak, the number of involved voxels and the peak F and pFWEcorr values. Therefore, other brain structures were involved in the clusters, especially in the large ones (see text).

<table>
<thead>
<tr>
<th>Anatomical region</th>
<th>X</th>
<th>Y</th>
<th>Z</th>
<th># of voxels</th>
<th>TFWEcorr</th>
<th>EC-AD T (p)</th>
<th>EC-SD T (p)</th>
<th>AD-SD T (p)</th>
</tr>
</thead>
<tbody>
<tr>
<td>L middle temporal pole</td>
<td>34</td>
<td>6</td>
<td>52</td>
<td>1005</td>
<td>12.84 (&lt;0.001**)</td>
<td>3.86 (&lt;0.001**)</td>
<td>5.54 (&lt;0.001**)</td>
<td>4.66 (&lt;0.01*)</td>
</tr>
<tr>
<td>R middle temporal pole</td>
<td>42</td>
<td>16</td>
<td>32</td>
<td>51</td>
<td>47.49 (&lt;0.001**)</td>
<td>2.83 (0.009)</td>
<td>6.61 (&lt;0.01*)</td>
<td>4.66 (&lt;0.01*)</td>
</tr>
<tr>
<td>L insula</td>
<td>−36</td>
<td>−10</td>
<td>−10</td>
<td>111</td>
<td>46.71 (&lt;0.001**)</td>
<td>3.65 (&lt;0.01*)</td>
<td>4.85 (&lt;0.01*)</td>
<td>3.37 (0.02)</td>
</tr>
<tr>
<td>L putamen</td>
<td>32</td>
<td>−12</td>
<td>−4</td>
<td>57</td>
<td>39.30 (&lt;0.001**)</td>
<td>7.14 (&lt;0.01*)</td>
<td>4.79 (&lt;0.01*)</td>
<td>4.54 (&lt;0.01*)</td>
</tr>
<tr>
<td>L globus pallidus</td>
<td>−12</td>
<td>6</td>
<td>−6</td>
<td>64</td>
<td>32.51 (&lt;0.01**)</td>
<td>4.72 (&lt;0.001**)</td>
<td>3.40 (0.02)</td>
<td>2.09 (0.1)</td>
</tr>
<tr>
<td>R inferior temporal gyrus</td>
<td>−58</td>
<td>−4</td>
<td>−30</td>
<td>66</td>
<td>27.22 (&lt;0.05*)</td>
<td>3.60 (&lt;0.01*)</td>
<td>4.14 (&lt;0.01*)</td>
<td>4.14 (&lt;0.01*)</td>
</tr>
<tr>
<td>L inferior temporal gyrus</td>
<td>−60</td>
<td>−18</td>
<td>−28</td>
<td>21</td>
<td>27.19 (&lt;0.05*)</td>
<td>4.26 (&lt;0.001**)</td>
<td>16.33 (&lt;0.001**)</td>
<td>6.51 (&lt;0.011**)</td>
</tr>
</tbody>
</table>

T-test crit.: p-value: p < 0.007; L, left; R, right.

Table 5
CBF-Event-related potential linear regression of the anatomical regions and the x-y-z coordinates that correspond to the MNI coordinates at the Tpeak, the number of involved voxels and the peak F and pFWEcorr values.

<table>
<thead>
<tr>
<th>Anatomical region</th>
<th>X</th>
<th>Y</th>
<th>Z</th>
<th># of voxels</th>
<th>TFWEcorr</th>
<th>EC-AD T (p)</th>
<th>EC-SD T (p)</th>
<th>AD-SD T (p)</th>
</tr>
</thead>
<tbody>
<tr>
<td>R middle temporal gyrus</td>
<td>44</td>
<td>−2</td>
<td>−2</td>
<td>30</td>
<td>21</td>
<td>5.61 (&lt;0.01**)</td>
<td>4.66 (&lt;0.01**)</td>
<td>4.66 (&lt;0.01**)</td>
</tr>
<tr>
<td>R inferior temporal gyrus</td>
<td>46</td>
<td>8</td>
<td>−40</td>
<td>28</td>
<td>5.60 (&lt;0.001**)</td>
<td>5.24 (&lt;0.001**)</td>
<td>4.79 (&lt;0.01*)</td>
<td>4.14 (&lt;0.01*)</td>
</tr>
<tr>
<td>L insula</td>
<td>−42</td>
<td>−2</td>
<td>−6</td>
<td>70</td>
<td>5.58 (&lt;0.001**)</td>
<td>5.24 (&lt;0.001**)</td>
<td>4.79 (&lt;0.01*)</td>
<td>4.14 (&lt;0.01*)</td>
</tr>
<tr>
<td>L superior temporal gyrus</td>
<td>−60</td>
<td>−4</td>
<td>−12</td>
<td>42</td>
<td>5.24 (&lt;0.001**)</td>
<td>5.24 (&lt;0.001**)</td>
<td>4.79 (&lt;0.01*)</td>
<td>4.14 (&lt;0.01*)</td>
</tr>
<tr>
<td>L superior temporal pole</td>
<td>−32</td>
<td>12</td>
<td>−28</td>
<td>13</td>
<td>5.09 (&lt;0.05)</td>
<td>5.24 (&lt;0.001**)</td>
<td>4.79 (&lt;0.01*)</td>
<td>4.14 (&lt;0.01*)</td>
</tr>
<tr>
<td>L middle temporal pole</td>
<td>−38</td>
<td>6</td>
<td>−36</td>
<td>36</td>
<td>4.82 (&lt;0.001**)</td>
<td>5.24 (&lt;0.001**)</td>
<td>4.79 (&lt;0.01*)</td>
<td>4.14 (&lt;0.01*)</td>
</tr>
<tr>
<td>L inferior temporal gyrus</td>
<td>−56</td>
<td>0</td>
<td>−32</td>
<td>24</td>
<td>4.49 (&lt;0.01)</td>
<td>5.24 (&lt;0.001**)</td>
<td>4.79 (&lt;0.01*)</td>
<td>4.14 (&lt;0.01*)</td>
</tr>
</tbody>
</table>

L, left; R, right.

to the linear regression of the N400 are reported. As such, seven clusters met the significance criteria of p < 0.0001, as well as the FWE correction (p < 0.05), at the cluster level (Table 5). The clusters mainly converged with those of the voxel-based CBF statistics, except for those in the left superior temporal gyrus (Fig. 5D). However, the left putamen and globus pallidus did not show any significant relationship between CBF and the N400. The individual CBF and N400 correlation values can be drawn from the scatter plots of each cluster (Fig. 6). While the SD group exhibited lower values in both domains, the EC group showed the opposite results and the values in the AD group were intermediate. This observation raised the question of whether the N400 correlation can be regarded as a putative marker for dementia. For this purpose, the sensitivity, as well as the specificity, of separating the participant groups was calculated. First, the 95% confidence intervals (CI) of the N400 correlation coefficients were derived for each group (CI for EC = 0.48–0.74; AD = 0.05–0.45; SD = −0.28–0.26). Thus, the CIs of the EC and the AD groups did not overlap. Therefore, the coefficients between 0.45 and 0.48 reflected the boundary between healthy participants and demented ones. Such a separation was not possible between the AD and SD groups. Consequently, each individual’s N400 correlation coefficient was compared with the cut-off values from 0.45 to 0.48 in the analysis (true positives = 15; false negatives = 4; true negatives = 15; false positives = 4). These results yielded a sensitivity and specificity of 0.79 each for all of the values between the CIs of the EC and AD groups because none of the participants had a N400 coefficient between 0.45 and 0.48. Taken together, these results showed that decreased N400 similarity can be considered an indication of dementia. In addition, the N400 similarity was related to reduced CBF in the circumscribed brain areas, demonstrating an association of the two neurophysiological measures. However, according to the present data, a distinction between the AD and SD groups was not feasible by the decrease in N400 similarity.

Correlations of the physiological parameters with the behavioral variables

Table 6 displays all of the correlation indices between the physiological and the neuropsychological test parameters. The most important result of this analysis was the significantly positive correlation of the N400 similarity with the MMSE score and especially with the semantic test scores for the BNT, AF, and VF. In addition, all four of these tests were positively correlated, as expected. The moderate positive correlation...
Fig. 6. Scatter plots for each cluster depicting individual N400 correlation (r) and cerebral blood flow. AD, Alzheimer's disease; EC, elderly controls; SD, semantic dementia.
of the fluency scores with the CT construction might reflect that these tests required executive functions for successful performance.

DISCUSSION

The results of the present study indicated that the N400 topography might be a measure that should be further investigated in order to identify a cost-efficient and non-invasive marker of dementia. Moreover, a correlation of the N400 similarity with decreased CBF in the anterior temporal lobes was found, and this reflected the underlying pathology. Specifically, the combination of altered electrophysiology (N400), which was closely related to the patients’ symptomatology as indicated by the positive correlations of the N400 similarity with the neuropsychological tests assessing semantic memory functions, with the neurophysiological aberrations (altered regional CBF) might help to further disentangle the pathological semantic memory processes in dementia. Before the crucial results involving the correlation of CBF and ERPs are discussed, other important findings in the voxel-based analyses, behavior, and ERPs are reviewed.

Voxel-based analyses (VBM and CBF)

The GM volume differences in the AD and SD groups compared to the EC group were mostly in line with previous findings [39–42, 44]. Besides the structural findings, the voxel-based CBF results showed that the anterior temporal lobes, in particular, were functionally altered in the AD and SD groups, as shown by decreased CBF. When comparing the number of significant voxels between each hemisphere, a moderate lateralization to the left can be observed. This applied primarily to the AD group, in which lowered CBF was found only in the left temporal poles, while lowered CBF was found bilaterally in the SD group. Taken together, for the AD group, these findings converge with those of earlier studies that investigated CBF changes [48, 50]. Conversely, no hypermetabolism was measured in the medial temporal lobes in the AD group, which differed from the findings of Alsop et al. [49]. One reason for this divergence could be the milder AD condition of the current group (MMSE = 24.8) compared to the group examined in Alsop’s study (MMSE = 22.2). Nevertheless, this is the first study that investigated (ASL) CBF at rest in patients with SD. Despite the lack of comparable studies, the resulting brain areas that exhibited reduced CBF were in line with the assumptions. For instance, they concurred with Diehl’s [52] findings about the decreased glucose metabolism in patients with SD.

Behavior

Besides the neurophysiological measures, the patients’ symptomatology is of importance, because it can be understood as the behavioral manifestation of the above-mentioned structural and functional cerebral aberrations. In the present study, the AD and SD groups were comprised of individuals in an early dementia stage (see MMSE scores). However, both the BNT as well as the VF/AF showed that they suffered from severe semantic word retrieval deficits. Yet most of the patients were able to perform the LD task and showed semantic priming, as shown by the shorter RTs for related word pairs compared to unrelated word pairs. This was in accordance with the findings of Rogers et al. [22], who showed associative semantic priming both in the AD and SD groups. Thus, these results indicated that, in those patients, at least the automatic semantic processes (i.e., spread of activation) were still functional [19, 76].

ERPs

By first focusing on the waveforms (Fig. 3), one could observe that the waveforms of for example the F3 and Pz electrodes in the AD and EC groups converged with those found in the study of Revonsuo et al. [33]. Thus, the notion of the preserved spread of activation was supported and further substantiated by the comparable P1 and N1 topographies in the AD (and SD) groups in contrast to the EC template in this study, although the patients’ correlation values were lower than those of the EC group. It was apparent that, for all ERPs, patients with SD exhibited the most deviant topographies, while those with AD showed intermediate topographic similarities that were between those of the EC and SD groups. The zero correlation of the SD group especially showed that there was no typical N400 topography present in this group, indicating severe deficits in controlled semantic word retrieval or a differing retrieval strategy. Thus, the current results indicated that the N400 separated the SD group from the AD and EC groups. However, the sensitivity and specificity analysis did not fully support this. Instead, it was found that the N400 correlation coefficient separated the healthy elderly from the patients with early dementia with a sensitivity and specificity of 0.79.
Hence, this result revealed that the N400 similarity was a putative marker for early dementia but not for a differential diagnosis of AD or SD. Of course, the fact that this result was based on a small participant group size, larger samples and especially longitudinal studies are needed in order to verify the current finding. For instance, the possibility cannot be excluded that either the false-positive EC participants will later develop dementia or those with low N400 similarity have decreased controlled semantic memory abilities in general.

In summary, it was surprising that the SD group showed comparable early ERPs as the EC and AD groups because a loss of semantic knowledge would have also led to an aberrant spread of activation. Therefore, it is noteworthy that this is the first study to detect P1 and N1 of semantic word processing in the SD group. This result suggested the preserved automatic processes in patients with AD [77, 78] and in patients with SD, which is an important finding for future studies and for clinical implications. Furthermore, when attempting to compare the current ERP findings to the existing literature, consistency was found in the altered N400 topography that was related to impaired semantic word retrieval in patients with AD and SD [29, 35, 37]. Nevertheless, the observation that the AD’s N400 topography still had a typical shape might indicate preserved semantic knowledge but impaired access, and this indication converges with those of Ford et al. [34] and Auchterlonie and colleagues [35].

Linear regression of CBF and ERPs

Contradicting the assumptions made in this study, neither the P1 nor the N1 topographies seemed to be related to changes in CBF. One reason might have been that the automatic spread of activation in the semantic network was not functionally changed in the patients, as discussed above. Opposed to this, the preserved N400 topography was associated with higher CBF, especially in the left temporal pole and the lateral temporal lobe, but also in the left insula and the right lateral temporal lobe. Congruous with the voxel-based results, the clusters in the temporal pole exclusively in the left hemisphere indicated a lateralization to the language-dominant hemisphere. Thus, the present results indicated that the controlled semantic word retrieval relied strongly on anterior temporal lobe functions. This view was supported by a study of Wirth et al. [25], which showed that the N400 is related to bilateral activation in the temporal lobes. Accordingly, the observations that the patients with SD showed severe GM atrophy in this region, dramatically reduced baseline blood flow and almost no N400 appeared consistent. Moreover, in patients with AD, GM volume loss was less extended, as was their CBF reduction. Therefore, the controlled semantic word retrieval was preserved to some degree, as expressed by the rather typical N400 topography, although it was altered compared to that of the EC group. Taken together, the potential of the N400 topography as an early marker for dementia was supported by its relationship to the structural and functional neuropathology in dementia, as was demonstrated in the present study and in recent studies (e.g., [36, 79, 80]).

CONCLUSION

The findings of the present study contributed to the understanding of the underlying mechanisms of semantic memory deterioration in patients with AD and those with SD based on three modalities: structure (GM volume), baseline metabolism (rest CBF), and task functionality (ERPs). In particular, these results showed a large overlap of reduced blood flow in the
brain areas that were affected by GM volume loss. Furthermore, deviant N400 topographies were associated with reduced CBF in most of these regions. Namely, the temporal lobes bilaterally, which trigger the N400 that is related to lexical-semantic integration [25, 81], appeared to play a crucial role in the interaction of atrophy, altered baseline blood flow, and impaired controlled semantic word retrieval.

Even though these results seem promising, the sole use of the N400 topography as an early marker for dementia is not yet applicable and needs replication in additional studies with independent participant groups. However, the high sensitivity of the N400 similarity may be a motivation for forthcoming studies to validate this marker in order to establish a cost-efficient and non-invasive diagnostic tool that complements those already available. To this end, future studies need to replicate and refine the current findings in order to support the use of the N400 for a differential diagnostic purpose. Moreover, with the prospect of improving the understanding and sensitivity of the ERPs, longitudinal studies are needed to elucidate the individual development of the early P1 and N1 and the late N400 topographies, ideally in the elderly who are healthy and those who convert to dementia. For instance, Bobes et al. [82] have reported that altered N400 topographies might occur even before the manifestation of semantic memory symptoms.

Other limitations of this study need to be considered. A major problem was the small group sizes, especially in the SD group. In particular, quite a few analyses showed tendencies to statistical significance, suggesting that more effects might have emerged with larger sample sizes. As such, a generalization of the present findings appeared difficult. Nevertheless, because SD is a relatively rare condition in the general population and is often not diagnosed, this sample was nevertheless of precious value. The fact that these five SD patients provided functional data in a task that was closely related to their cognitive deficits, as well as the structural and baseline blood flow images, makes this notion even stronger. Finally, it has to be examined whether the N400 similarity is specific for patients with dementia or is also found in patients with other disorders.

In conclusion, the present study demonstrated that the altered N400 electrophysiology in patients with dementia with semantic memory impairments was closely related to their structural and baseline blood flow degeneration, and this was found distinctly in regions that are involved in controlled semantic word processing.

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REFERENCES


